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Using an Augmented Reality Device as a Distance-Based Vision Aid – Promise and Limitations

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Abstract

Significance: For people with limited vision, wearable displays hold the potential to digitally enhance visual function. As these display technologies advance, it is important to understand their promise and limitations **as vision aids**.

Purpose: Test the potential of a consumer augmented reality (AR) device for improving the functional vision of people with near-complete vision loss.

Methods: An AR application that translates spatial information into high contrast visual patterns was developed. Two experiments assessed the efficacy of the application to improve vision: an exploratory study with four **visually impaired** participants, and a main controlled study with participants with simulated vision loss (N = 48). In both studies, performance was tested on a range of visual tasks (identifying the location, pose and gesture of a person, identifying objects, and moving around in an unfamiliar space). Participants' accuracy and confidence were compared on these tasks with and without augmented vision, as well as their subjective responses about ease of mobility.

Results: In the main study, the AR application was associated with substantially improved accuracy and confidence in object recognition (all P s < 0.001) and to a lesser degree in gesture recognition (P < 0.05). There was no significant change in performance on identifying body poses, or in subjective assessments of mobility, as compared to a control group.

Conclusions: Consumer AR devices may soon be able to support applications that improve the functional vision of users for some tasks. In our study, both artificially impaired participants and participants with near-complete vision loss performed tasks that they could not do without the AR system. Current limitations in system performance and form factor, as well as the risk of over-confidence, will need to be overcome.

Keywords: **augmented reality; assistive devices; low vision and blindness**

1 For the millions of people who are affected by low vision and blindness, independence and
 2 mobility pose daily challenges.¹⁻³ To address these challenges and improve the functional vision
 3 of this population, a range of assistive tools have been developed, including vision aids and
 4 sensory substitution devices. Recently, available tools have included custom head-mounted
 5 display (HMD) systems designed to digitally enhance visual information, such as Jordy (Enhanced
 6 Vision, Huntington Beach, CA), LVES,⁴ eSight (eSight, Toronto, ON), and NuEyes (NuEyes,
 7 Newport Beach, CA). The basic principle of these HMDs is to substitute the image cast by the
 8 world on the retina with an enhanced view. Outward-facing cameras capture live video of the
 9 world in front of the user; this video is processed to increase visibility via magnification or contrast
 10 enhancement, and then shown in (near) real-time to the user through a pair of micro-displays
 11 positioned in front of the eyes.⁵⁻⁷ This is called a ‘video see-through display’ because although the
 12 system is mobile, the users’ eyes are covered by opaque screens. While these systems are
 13 promising and can measurably increase functional vision,⁶ they also tend to suffer from temporal
 14 lag, cumbersome hardware, and reduced visual field. To date, no video see-through system has
 15 been widely adopted.

16 At the same time, HMDs have emerged as a popular platform for mass consumer
 17 electronics, with a range of companies selling these systems to general consumers for virtual and
 18 augmented reality (VR/AR) applications. In particular, *optical* see-through AR systems – such as
 19 Glass (Google, Mountain View, CA) and HoloLens (Microsoft, Redmond, WA) – can augment
 20 vision without having to cover the eyes with an opaque screen. These commercial products also
 21 benefit from the cost-savings of mass production, improvements in form factor, and the ability to
 22 flexibly support a range of software applications (“apps”). Despite the lower contrast typical of
 23 see-through displays, these AR systems have several potential advantages compared to *video*
 24 see-through displays. For example, the user’s natural field of view is intact, and their eyes are un-
 25 occluded. Thus, the incorporation of assistive features into a consumer AR system provides a
 26 potential new avenue for broadening the impact of this technology on the low vision and blind

27 population, much like consumer smartphones have broadened the availability of hand-held
28 assistive tools.⁸

29 One early study used off-the-shelf HMDs to build a see-through visual multiplexing device
30 for visual field loss,⁹ but at the time additional custom hardware was required to achieve the
31 desired effect. A more recent study examined visual acuity and sensitivity for text and shapes
32 presented on a see-through AR system, showing that a variety of virtual content can be visible to
33 **visually impaired** users on a consumer system.¹⁰ However, no specific assistive applications were
34 explored. Another recent study showed that overlaying enhanced edge information on a see-
35 through HMD can increase contrast sensitivity in simulated visual impairment.¹¹ Here, we build
36 on this prior work to examine alternative avenues for visual enhancement using consumer AR.

37 The question how best to augment visual information is still an open one.^{5, 12-14} Particularly
38 in complex natural environments, overall edge or contrast enhancement may not make individual
39 objects and elements easier to perceive for individuals with near-complete vision loss (**i.e.,**
40 **individuals with severely impaired vision or legal blindness**).¹⁵ Instead, selectively enhancing only
41 the edges that indicate object boundaries may simplify complex visual patterns so as to help
42 people with severely impaired vision parse natural scenes.¹⁶⁻²⁰ In particular, a few previous studies
43 have employed a 'distance-based' enhancement system that translates the distance of points in
44 front of the user into pixel brightness values, and showed that visually impaired users wearing
45 this video system could perform a visual search task while seated,¹⁶ and collided with fewer
46 obstacles in a mobility task.²¹ **A similar approach was recently implemented in a custom-built see-**
47 **through system.**²² Here, we examine the ability of emerging consumer AR hardware (**Figure 1**)
48 to implement a similar distance-based visual augmentation, with a focus on usability for
49 individuals with near-complete vision loss. **We focus on this group specifically because prior work**
50 **and our own pilot testing suggest that they may be the most likely to find utility in distance-based**
51 **information. Thus, we test the hypothesis that distance-based AR can improve functional vision**
52 **in this target population for a range of tasks.** We develop an application to run on the HoloLens

53 that translates spatial information from the physical environment into an AR view containing
54 simplified patterns with high-contrast edges between objects at different distances. We then
55 examine the impact of the application on performance of a range of visual tasks in an exploratory
56 study with visually impaired users ($N = 4$) with a range of etiologies, and in a main study using a
57 larger sample ($N = 48$) of people with simulated visual impairment. We focus on understanding
58 existing strengths, areas of potential, and current limitations.

59

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Figure 1 about here.

61 Methods

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63 Hardware

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The HoloLens is a head-mounted AR system that can display 3D virtual surfaces within the physical environment.²³ The system includes two see-through displays that subtend approximately 30° horizontally and 17.5° vertically in each eye (**Figure 1A**, red arrows). A set of sensors (**Figure 1A**, blue dashed box) – including four scene-tracking cameras, an infrared-based depth sensor, and an inertial measurement unit – continuously track the user’s position and orientation in the environment. As the user moves around, the HoloLens also measures and stores the dimensions and shape of the physical space around them, creating a 3D reconstruction of the surrounding environment. This 3D reconstruction is provided to developers as a triangle mesh, in which the number of individual triangles used to define the environment per unit area determines the resolution and detail of the 3D map. User input is accepted via multiple channels, including speech, hand gestures, and Bluetooth devices. All computation is completed on board, so the system is untethered (**Figure 1B**) and has a battery life of 2-3 hours with active use. It weighs approximately 580 grams.

78 Application development

79 Software development was performed using Microsoft's HoloToolkit and Unity (Unity
80 Technologies, San Francisco CA, USA). We developed an application that measures the distance
81 of surfaces and objects in the environment from the user by accessing the user's position and the
82 3D environment map. The application discretizes these distances into a set of bands, each with
83 a unique color and intensity value. The bands are directly overlaid **semi-transparently** on the
84 environment in stereoscopic 3D when viewed through the displays (**Figure 2A,B**), creating an AR
85 environment that is a mixture of real and virtual surfaces. The AR environment has a simplified
86 visual geometry, with high contrast-edges between objects and surfaces at different distances
87 from the observer, which we hypothesize is more easily interpretable by people with impaired
88 vision relative to the original view.^{16, 17, 19} **When using the system, the natural field of view is**
89 **unrestricted, so the appearance is similar to having a window into the AR environment through**
90 **the HoloLens display (see above).** As the user moves around the environment, the colors change
91 to reflect the distances from the current viewpoint. The mapping between distance and color is
92 arbitrary. We created 18 unique mappings to enable customization for different levels of visual
93 impairment and color vision (**Figure 2C** shows 9 examples). Some mappings transition between
94 two colors from high to low saturation (left column); some transition from white to one color (middle
95 column) and some transition from high to low opacity (right column). Because the HoloLens
96 displays can produce light but cannot occlude it, transitions from white to black are not possible.
97 In addition, the overall **luminance** and opacity of the overlays is adjustable, which is useful for
98 cases in which a user is particularly light sensitive, **or for transitioning between environments with**
99 **differing ambient light levels.** The source code for our application is freely available for research
100 purposes.

101

102

Figure 2 about here.

103

104 In Experiment 1, we allowed users to select any one of the 18 mappings that created the
105 most visible contrast between the foreground and background of a scene. In Experiment 2, we
106 used two different mappings (red-to-blue, shown in **Figure 2B**, and high-to-low opacity). In both
107 experiments, the update rate for the display and motion tracking was set to 60 Hz, and **the**
108 **resolution of the 3D environment mesh was set to the highest density that produced noticeable**
109 **improvements in 3D detail (~2000 triangles per cubic meter). There was a one second delay**
110 **between subsequent mesh updates, which was necessary for the system to scan and process**
111 **the updated mesh. Thus, all visual identification tasks were performed with the target person,**
112 **object, or gesture held stationary. Due to the fast tracking of user-generated motion, there was**
113 **no noticeable lag associated with body or head movements.**

114 The number of discrete color bands was set to 10 and distances closer than 0.5 m were
115 not augmented, so as not to impede near-vision. In Experiment 1, the first band covered 0.5 m to
116 1.5 m, the eight middle bands were each 0.25 m wide, and the final band covered distances
117 beyond 3.5 m. In Experiment 2, the first band extended to only 1.0 m, and all other bands were
118 also moved closer by 0.5 m accordingly.

119 Experiments

120 All participants in both experiments gave written informed consent and were compensated. The
121 procedures were approved by the Dartmouth College Institutional Review Board and comply with
122 the Declaration of Helsinki. The procedures and main hypotheses of Experiment 2 were
123 preregistered on AsPredicted.org (#2870). **For clarity, Table 1 provides a summary of the**
124 **participants, tasks, and number of trials conducted in each experiment.**

125

126

Table 1 about here.

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129

130 Experiment 1: Exploratory study with visually impaired participants

131 Participants

132 Four participants were recruited via an email advertisement. **Table 2** provides individual
 133 information about each participant. Note that Participant 4 works as a professional accessibility
 134 services manager. Participants were recruited with a range of conditions causing generalized
 135 vision loss and in some cases, visual field restriction.

136

137 *Table 2 about here.*

138

139 Customization

140 The experimenter calibrated the HoloLens for each participant in a two-step procedure.
 141 First, all pixels were turned on uniformly, and the device was adjusted to make sure that the
 142 displays were visible and the overall brightness was at a comfortable level. Next, the experimenter
 143 stood 1.5 m from the participant and turned on an initial color setting. The participant looked
 144 around and determined whether they could visually identify the location and shape of the
 145 experimenter’s body. At this stage, each participant indicated that they could see the
 146 experimenter. We then interactively determined the color setting that created the strongest
 147 perceived contrast between foreground and background. Finally, the experimenter stepped slowly
 148 backwards to confirm that the visible contrast changed with distance. **While this approach limited
 149 our ability to combine results across participants, due to the range of visual system pathologies
 150 present, it maximized the potential impact for each individual.** Of the four participants, one
 151 selected red-to-blue (Participant 1), two selected yellow-to-blue (Participants 2 and 3), and one
 152 selected white-to-blue (Participant 4).

153

154 Tasks

155 We conducted four naturalistic tasks, each consisting of two blocks of five trials. The first
 156 block was completed with the AR turned off (baseline) and the second block with the AR on, and

157 the trial order within each block were pseudo-randomized. Participants' performance
158 (correct/incorrect) and confidence (from 1 "it's a guess" to 3 "very certain") were recorded for each
159 trial. Tasks were selected to represent different levels of difficulty in visual identification, as well
160 as mobility. Participants performed all tasks in an indoor space with typical overhead lighting.
161 Prior to starting each task, participants performed a brief practice both with and without visual
162 augmentation.

163 *Person localization:* Participants sat in a chair and a life-size cutout figure of a person was
164 placed 1.8 m away from them. The location of the figure was pseudo-randomly assigned to one
165 of five positions (-45.0°, -22.5°, 0.0°, 22.5°, 45.0° from 'straight ahead'). On each trial in the
166 baseline and AR blocks, the participants indicated the location of the figure using a laser pointer.
167 The experimenter scored hits (1), near misses (0.5, the laser pointer missed the cut-out figure
168 only slightly) and misses (0). After each trial, participants rated their confidence.

169 *Pose recognition:* On each trial, the experimenter stood 1.5 m from participants and held
170 their arms in one of five different poses (arms straight out to the side, arms up forming a "Y," arms
171 above the head forming an "O," one arm straight up / one arm straight down, one arm bent down
172 at elbow / one arm bent up at elbow). The experimenter wore a black long-sleeve jacket and the
173 wall behind them was beige with some decorations, so that there was high contrast between the
174 foreground and background even without any augmentation. Participants mirrored each pose with
175 their arms and indicated their confidence. The response was recorded with a photograph and
176 later scored by a naïve judge on a 3-point scale with 0 indicating incorrect, 0.5 partially correct,
177 and 1 fully correct.

178 *Object recognition:* Participants identified objects that were placed one at a time on a table
179 1.5 m in front of them, and reported their confidence. The objects were a spray bottle, table lamp,
180 square wicker basket, recycling bin, and fake plant (**Figure 3A**). Prior to starting the task,
181 participants were given time to touch and look at each of the objects and identify them verbally.

182 To control for memory effects, the experimenter read aloud the list of objects before each block.

183 Participants responses were scored as either incorrect or correct.

184 *Mobility:* Participants walked forward from a fixed location and stopped when they
 185 identified an obstacle in their path (a white portable room divider 1.7 × 1.6 m). All participants
 186 except Participant 4 completed the task without a cane. In each trial, the obstacle was placed at
 187 a pseudo-randomly selected location between 5.5 m and 7.5 m from the starting position. After
 188 participants stopped, the experimenter measured the distance between them and the obstacle
 189 using a laser range finder. Confidence scores were not collected, because participants were
 190 instructed to stop as soon as they detected the obstacle.

191

192 Experiment 2: Controlled experiment with simulated vision loss

193 Sample

194 Forty-eight participants (mean age: 21.15, 34 female) were recruited, all with normal or
 195 corrected-to-normal visual acuity (0.00 logMAR or better) and normal stereoacuity (70 arcsec or
 196 better) assessed with a Randot Stereo Test (Precision Vision, LaSalle, IL, USA). During all tasks,
 197 participants wore a pair of swim-goggles modified binocularly with Bangerter occlusion foils (type
 198 LP; Ryser Optik, St. Gallen, Switzerland), which degrade visual acuity uniformly across the visual
 199 field²⁴. The LP-type foils simulate visual acuity at the level of perceiving hand movements, with
 200 some rough shapes and forms distinguishable under typical indoor lighting. For each participant,
 201 we verified that the simulators resulted in letter acuity less than 1.60 logMAR (approx. 20/800),
 202 inability to count fingers at 1.0 m, and intact perception of hand movements. One session was
 203 repeated due to technical errors.

204

205 Conditions

206 Participants were randomly assigned to one of three groups ($n = 16$). In the *color group*,
 207 the red-to-blue AR color mapping was used (**Figure 2B**). In the *opacity group*, the bands had
 208 differing levels of opacity: near distances were most opaque and distances beyond the 9th band

209 were fully transparent. In the *control group*, participants were told that the HoloLens would
 210 augment their vision, however, no actual augmentation was displayed (at the start of each task
 211 for which vision was supposed to be augmented, the HoloLens screen flashed blue and faded
 212 back to being fully transparent). This group was included to examine potential practice effects or
 213 increases in effort/attention associated with the knowledge of augmented vision.

214

215 Visual identification tasks

216 Participants performed three identification tasks, each consisting of two blocks of six trials
 217 (the first block with the AR turned off and the second block with the AR on). The overall procedure
 218 used was the same as the exploratory study, but the study was carried out in a different location
 219 and with some differences in the tasks. Three naïve judges scored pose and gesture recognition
 220 accuracy and their ratings were averaged to determine the final score.

221 *Pose & object recognition:* These tasks were performed in the same manner as described
 222 in Experiment 1, with the exception that the viewing distance for poses was 2.2 m. A sixth pose
 223 (“both arms straight up”) and object (stack of books) were also included. The inter-rater reliability
 224 of the scoring for poses was 0.78 (Fleiss Kappa), suggesting substantial agreement (defined as
 225 0.61-0.80).²⁵

226 *Gesture recognition:* To assess the spatial resolution of the augmented vision, the
 227 experimenter stood 1.2 m from the participants and made one of six gestures with their right hand
 228 held to their side (thumb-up, shaka [“hang loose”], open palm, fist, peace sign, okay). The
 229 participants mirrored the hand gesture and indicated their confidence. Responses were scored
 230 as for the poses and inter-rater reliability was 0.63.

231

232 *Figure 3 about here.*

233

234 Mobility task

235 Participants explored a room (5.3 m × 3.6 m) with an unknown layout in three trials. On
236 each trial, the furniture in the room was arranged in one of three different layouts (selected
237 pseudo-randomly) and the participants were given 60 sec to complete the task (**Figure 3B**). On
238 the first trial, the AR remained off (baseline). **There were two test trials: one in which the AR was**
239 **on, and another in which a white cane was used as an assistive tool. The ordering of these two**
240 **trials was determined pseudo-randomly.** Prior to the cane trial, participants practiced using the
241 cane in a different room. After each trial, participants rated their level of agreement on a scale of
242 1 (strongly disagree) to 7 (strongly agree) with four statements: “Overall, I felt comfortable while
243 exploring the room”, “I felt unlikely to run into things”, “It was easy to navigate the space”, and “I
244 felt that my vision provided useful information”. After all trials, participants indicated whether
245 baseline, AR, or cane was the best with respect to each of these statements. Since we used the
246 same room with different layouts, the HoloLens’ storage of overlapping spatial meshes could
247 cause technical issues. Thus, between trials we cleared the system memory and circled the room
248 once to orient the system to the new layout (note that this problem does not occur if the system
249 is moved to a new room).

250

251 Data analysis

252 All data were analyzed using the R Environment for Statistical Computing, version 3.3.2.²⁶
253 For Experiment 1, in some cases participants were unable to detect any visual information during
254 the baseline trials and did not provide guesses. On these trials, confidence was scored as zero
255 (note that this was the case for all baseline trials for Participant 4). For Experiment 2, effects of
256 the independent variables (*experiment group* [control/color/opacity] between subjects, and *trial*
257 *block* [baseline/AR] within subjects) were assessed using repeated measures ANOVAs
258 (significance level of $P < 0.05$). For post-hoc analyses, p-values were Bonferroni corrected.
259 Normality of data **from Experiment 2** were tested using Shapiro-Wilk tests. For gesture and pose

260 recognition in Experiment 2, analyses were performed on the average accuracy ratings of the
261 three judges. Due to technical errors, data from one trial in Experiment 1 and one trial in
262 Experiment 2 were not recorded. The raw response data and analysis code are provided on
263 publicly accessible repositories.

264 Results

265

266 Experiment 1

267 Accuracy and average confidence ratings for each of the four participants in the visual
268 identification tasks are shown in **Figure 4A-C**. Each pair of colored bars shows the results for an
269 individual participant's baseline and AR trials. Participants 1, 2 and 3 were able to complete the
270 person localization task consistently both with and without AR, and reported high confidence
271 (**Figure 4A**). Participant 3 (brown bars) indicated after the task that the augmentation made her
272 more confident (despite her ratings being similar). However, Participant 1 (magenta bars)
273 remarked that the checkered shirt of one experimenter was actually more visible without the
274 augmentation. Participant 4 (yellow bars) was unable to locate the figure without AR, but correctly
275 located it on 80% of trials with AR, with medium confidence. Similar patterns were observed for
276 pose recognition (**Figure 4B**). Participants 1 and 2 performed the task with high accuracy and
277 confidence, but for this task Participant 3 had lower accuracy overall (compared to person
278 localization), and reported higher confidence with AR. Participant 4 was unable to perform the
279 task at baseline, but obtained reasonably accurate performance (with low confidence) with AR.
280 **Qualitatively**, all but Participant 2 improved in object recognition in the AR block (**Figure 4C**),
281 while Participant 2 decreased slightly both in performance and confidence.

282

283 *Figure 4 about here.*

284

285

286 The results for the mobility task are shown in **Figure 4D**, in terms of the average distance
287 each participant required to detect the obstacle and stop walking. In most trials without AR,
288 Participants 1, 2, and 3 detected the obstacle one or two steps before reaching it. Participant 1
289 detected the obstacle on average at a similar distance in the baseline and AR blocks (1.4 and 1.6
290 m). However, he reported using a different strategy in the two conditions: in the baseline trials, he
291 used the contrast between the obstacle and the background, when using AR, he instead relied
292 on the color-distance information. This participant also indicated that the augmentation worked
293 well for him to identify walls, and used it to guide himself to stop each time he returned to the
294 starting position. Participants 2 and 3 both tended to detect the obstacle in the AR block from
295 approximately 3 m, which roughly matches the onset distance of the farthest color transition;
296 however, Participant 3 indicated that using a cane would be simpler. Participant 2 walked fastest,
297 and on some trials experienced issues with the color map not updating quickly enough. Participant
298 4 could not detect the obstacle visually at baseline, so he used his cane. In one baseline trial and
299 one AR trial, the participant changed direction prior to reaching the obstacle and thus never
300 located it. However, on each of the AR trials, he detected the obstacle visually before hitting it
301 with his cane, with an average distance of 1.88 m.

302

303 **Other responses**

304 Participants also reported on the strengths and weaknesses of the application and the
305 hardware after completing all tasks. Participant 1 stated that if the hardware had the same form
306 factor as a pair of glasses, it would be useful, and that providing distance information relative to
307 the head was preferable for him than receiving this feedback on other parts of the body (like the
308 arm). Overall, he said the system was somewhere between distracting and helpful. Participant 2
309 stated that overall his vision was worse with the overlays, and that the lag time was a problem (as
310 we observed during the mobility task). Participant 3 also expressed that the current form factor of
311 the system was undesirable, but that she might find the system particularly helpful at night.

312 Participant 4, whose vision was more strongly impaired than the others' and most improved when
 313 using the AR system, noted that he had to move his head around more in the identification tasks.
 314 **This may reflect the limited display size in the visual field.** However, unlike the other participants
 315 he indicated that the device was comfortable as is and that the form-factor was not an issue.

316 Overall, these results suggest that improvements in functional vision (particularly for object
 317 identification and obstacle detection during mobility) may be achievable with the AR system, but
 318 indicate that the usefulness of the distance-based augmentation likely varies by task and visual
 319 ability. In addition, these results on their own do not rule out the possibility that any objective or
 320 subjective changes in vision could be due to increased attention, effort, or practice during the
 321 trials with augmented vision, due to the novelty of using AR.

322
 323 **Experiment 2**

324 In this main study, we examined the potential changes in functional vision created by the
 325 AR system in a larger sample of participants with simulated near-complete vision loss. We also
 326 examined the potential impact of the system novelty on our measures of performance by inclusion
 327 of **a control group**.

328
 329 **Visual identification tasks**

330 The results from each of the three visual identification tasks for mean accuracy (top row)
 331 and confidence (bottom row) are shown in **Figure 5**, separately for the *control group* (gray bars),
 332 *color group* **and** *opacity group* (**orange** bars). Recall that the procedure for the *baseline* blocks
 333 (light shaded bars) was identical for each group, so variability across groups can be attributed to
 334 random variance, and that the *control group* was told they would have augmented vision, but after
 335 a brief flash the HoloLens display was actually turned off. The three tasks were selected to range
 336 from easy (pose recognition) to difficult (object and gesture recognition) when performed at
 337 baseline. This is reflected by the fact that baseline accuracy and confidence are overall high for
 338 pose recognition and relatively low for object and gesture recognition. A useful vision aid should

339 ideally improve performance on tasks that are challenging, but importantly, it should also not
 340 degrade performance on tasks that are already easily accomplished with un-augmented vision.

341

342 *Figure 5 about here.*

343

344 First, we examine the effect of the augmentation on accuracy on each task. For pose
 345 recognition (**Figure 5A**), there were no significant main effects or interaction **terms** for
 346 experimental group (*control/color/opacity*) or trial block (*baseline/AR*) variables (*experiment*
 347 *group: $F(2,45) = 0.72, P = 0.49, \eta_p^2 = 0.03$; trial block: $F(1,45) = 0.82, P = 0.37, \eta_p^2 = 0.02$;*
 348 *interaction: $F(2,45) = 0.15, P = 0.86, \eta_p^2 = 0.01$). Thus, while performance did not significantly*
 349 *improve with AR on this task, it also did not get worse. This is not entirely surprising, because*
 350 *performance was already quite high at baseline due to the high visual contrast (average percent*
 351 *correct across all groups was 61.3%). For object recognition (**Figure 5B**), significant main effects*
 352 *of experiment group and trial block were mediated by a significant interaction **term** ($F(2,45) =$*
 353 *13.01, $P < 0.001, \eta_p^2 = 0.37$). Post-hoc comparisons showed that performance improved*
 354 *significantly during the AR block in the *color* and *opacity* groups, but not in the *control* group*
 355 *(*control: $t(95) = 0.18, P = 0.86, d = 0.03$; color: $t(95) = 7.59, P_{corrected} < 0.001, d = 1.10$; opacity:**
 356 *$t(95) = 7.36, P_{corrected} < 0.001, d = 1.06$). Similarly, there was a significant interaction **term** ($F(2,45)$*
 357 *$= 3.66, P < 0.05, \eta_p^2 = 0.14$) in the gesture recognition task (**Figure 5C**), reflecting the fact that*
 358 *participants in the *opacity* group performed better in the AR block ($t(95) = 2.88, P_{corrected} < 0.05, d$*
 359 *$= 0.42$). This suggests that participants were able to use the information provided by the*
 360 *augmented vision to more accurately perceive the shape of the objects and the form of a hand*
 361 *gesture. In the case of gestures, the improvement was minor and likely not of practical use. For*
 362 *objects however, this improvement was substantial: the average percent correct was 65.0% using*
 363 *AR as compared to 19.4% without (over six trials). This is a promising amount of improvement,*
 364 *particularly considering that the level of simulated visual impairment was so severe. The ability to*

365 reliably recognize everyday objects visually with this system thus represents a practical
 366 improvement in functional vision.

367 Similar to the accuracy results, confidence ratings showed that participants overall rated
 368 their confidence to be highest in the pose recognition task and lowest in the object and gesture
 369 tasks. The confidence ratings for poses are shown in **Figure 5D**. As with accuracy, there were no
 370 significant main effects or interaction **terms** (*experiment group*: $F(2,45) = 0.64, P = 0.53, \eta_p^2 =$
 371 0.03 ; *trial block*: $F(1,45) = 1.32, P = 0.26, \eta_p^2 = 0.03$; *interaction*: $F(2,45) = 1.06, P = 0.35, \eta_p^2 =$
 372 0.05). For object recognition (**Figure 5E**), however, significant main effects were again mediated
 373 by a significant interaction **term** ($F(2,45) = 5.55, P < 0.01, \eta_p^2 = 0.20$). Participants reported higher
 374 confidence during the AR block in both the *color* and the *opacity* groups, but not in the *control*
 375 group (*control*: $t(95) = 2.01, P_{corrected} = 0.19, d = 0.29$; *color*: $t(95) = 6.75, P_{corrected} < 0.001, d =$
 376 0.97 ; *opacity*: $t(95) = 8.30, P_{corrected} < 0.001, d = 1.20$). Finally, confidence ratings for gesture
 377 recognition (**Figure 4F**) also showed a significant interaction **term** ($F(2,45) = 3.48, P < 0.05, \eta_p^2 =$
 378 0.13), reflecting higher confidence in the AR block in the *color* and *opacity* groups (*color*: $t(95) =$
 379 $4.94, P_{corrected} < 0.001, d = 0.71$; *opacity*: $t(95) = 5.39, P_{corrected} < 0.001, d = 0.78$).

380 These results show that participants tended to be more confident in the two more difficult
 381 tasks when using the AR system. This makes sense for object recognition, in which their
 382 performance improved with AR. The confidence that a user has with their augmented vision likely
 383 plays a key role in how willing they are to rely on visual information and perform tasks
 384 independently. It is interesting that confidence increased for gesture recognition as well, because
 385 performance was only modestly impacted. In the next section, we report an exploratory analysis
 386 assessing the possibility that using augmented vision might produce overconfidence: an increase
 387 in confidence even when perceptual judgments are incorrect. In this and subsequent analyses,
 388 we combine the two test groups (*color/opacity* are grouped together as *test*), because the pattern
 389 of results were highly similar.

390

391 Confidence as a function of performance

392 In all visual identification tasks, confidence ratings and performance were significantly
393 positively correlated (poses: $r = 0.53$, $P < 0.001$; objects: $r = 0.43$, $P < 0.001$; gestures: $r = 0.17$,
394 $P < 0.001$). **Figure 6** shows the average confidence ratings for each task separately for trials in
395 which participants gave correct or incorrect responses (for pose and gesture recognition, trials
396 with a score greater than 0.75 were categorized as “correct”, trials with scores lower than 0.25
397 were categorized as “incorrect”). Across all tasks, experiment groups, and trial blocks, participants
398 tended to report higher confidence in trials in which they gave correct answers. Interestingly,
399 partially overlapping t-tests (Bonferroni corrected for 12 comparisons; note that the number of
400 observations in each bin varied) revealed that participants in the *test* groups reported higher
401 confidence in the AR block, even when they gave incorrect answers (orange bars).²⁷ The only
402 exception is the incorrect trials for pose recognition (**Figure 6A**). This overconfidence was not
403 observed in the *control* group (gray bars). This underscores the importance of considering how to
404 provide feedback and training to help users understand how reliable their vision is when they use
405 an unfamiliar assistive device.

406

407 *Figure 6 about here.*

408

409 Mobility task

410 **Figure 7** shows the results from the participants’ responses after the mobility task. Rather
411 than detect a single obstacle, in this task participants were given time to freely explore an
412 unfamiliar room. For simplicity, responses are plotted as difference scores by subtracting out each
413 participant’s response in the baseline trial. Overall, these results show that reported
414 improvements were similar across both the *control* and *test* groups, suggesting that the subjective
415 assessments used in this task did not measure any potential effects of the AR system on mobility.
416 In both the *control* and *test* groups, participants tended to report feeling less likely to collide with

417 obstacles when using a cane and when using AR (**Figure 7A**). An ANOVA revealed only a main
 418 effect of trial type (*trial type [baseline/cane/AR]: $F(2,92) = 22.72, P < 0.001, \eta_p^2 = 0.33$; experiment*
 419 *group [control/test]: $F(1,46) = 0.02, P = 0.89, \eta_p^2 < 0.01$; interaction: $F(2,92) = 0.80, P = 0.45, \eta_p^2$*
 420 *= 0.02*), and differences relative to baseline were statistically significant for all conditions except
 421 when the control group used the cane (*test/AR: $t(31) = 3.45, P_{corrected} < 0.01$; test/cane:*
 422 *$t(31) = 6.01, P_{corrected} < 0.001$; control/AR: $t(15) = 3.76, P_{corrected} < 0.01$; control/cane: $t(15) = 2.31,$*
 423 *$P_{corrected} = 0.14$*). When comparing collision risk, 65.5% of the *test* group preferred the cane and
 424 34.5% preferred AR. In the *control* group, 56% and 38% preferred the cane and AR, respectively.
 425 Similarly, participants in both groups tended to report that their vision was more useful with AR
 426 (**Figure 7B**). There was also a main effect of trial type on these responses (*trial type: $F(2,92) =$*
 427 *13.14, $P < 0.001, \eta_p^2 = 0.22$; experiment group: $F(1,46) = 0.10, P = 0.76, \eta_p^2 < 0.01$; interaction:*
 428 *$F(2,92) = 0.45, P = 0.64, \eta_p^2 = 0.01$*), which reflected a statistically significant increase in both
 429 groups when using AR (*control: $t(15) = 3.65, P_{corrected} < 0.01$; test: $t(31) = 0.10, P_{corrected} < 0.01$*).
 430 When comparing usefulness of vision, 78.1% of the *test* group and 62.5% in the *control* group
 431 reported that AR was preferred. Because the *control* group experienced no real augmentation,
 432 these results together indicate that subjective ratings are likely an unreliable measure of mobility
 433 improvements in AR. For the two other statements (“Overall I felt comfortable while exploring the
 434 room.”, “It was easy to navigate the space.”), no significant effects of using a cane or AR were
 435 found.

436 *Figure 7 about here.*

437

438 Discussion

439 The advent of mass-market consumer AR systems, together with the rapid development
 440 of assistive mobile technology, holds substantial promise for visually impaired individuals.
 441 Although the diversification and increased availability of high-tech tools might assist and one day

442 even eliminate the need for biological vision in performing many day-to-day tasks, the precise
443 potential benefits and challenges are still unclear. Here, we present two experiments using an
444 application developed and deployed on a consumer AR device, which provides high-contrast,
445 customizable distance information overlaid in the user's field of view. The results suggest areas
446 in which current AR systems may be used to improve functional vision, and where they fall short.

447 Overall, our findings support previous work that simplifying visual scenes can be helpful
448 for people with severely impaired vision, and show that this approach can be implemented in a
449 see-through HMD display.^{16, 17, 19, 21} However, our studies indicate that the utility of the current
450 system varies substantially as a function of task. Experiment 1 also suggests that this particular
451 system may not be desirable in all forms of vision loss, both because visual detail from surface
452 texture can be lost, and because the resolution of the HoloLens 3D spatial mesh is limited. This
453 does not preclude the potential utility of AR for these users, who may instead benefit from overall
454 edge or contrast enhancement.¹¹ The flexibility of consumer devices provides a potential platform
455 to create a variety of applications from which a selection can be made depending on a user's level
456 of visual ability. However, the type of applications that are possible, and how they should differ
457 for different users, is an area that requires further research. Although low vision and blindness
458 simulators are frequently employed to examine task performance in controlled settings,^{11, 28, 29}
459 future work should examine systematically how the acuity levels and visual field loss associated
460 with specific etiologies may be addressed with AR.

461 Major limitations of the current HoloLens system include the fact that it only updates
462 distance information at up to 1 Hz, so visual perception of fast moving objects may be degraded.
463 However, the display can provide low-latency self-motion information because it builds up a stable
464 3D map as the user moves around a stationary environment. Nonetheless the lag and limited
465 range of the mapping are clear limitations of the device, which will hopefully improve with the next
466 generations of HMDs. As 3D sensing technologies improve, the ability to quickly update both self
467 and environmental motion will be essential. At the same time, the portion of the visual field

468 covered by the see-through display of the HoloLens is quite limited (30° horizontally). Key
469 information for several activities, such as navigation, may often fall in the peripheral visual field,
470 so improvements in the display size are highly desirable. In addition, the distance-based nature
471 of the current system means that regions of high visual contrast but low depth variance would
472 likely be degraded visually. Future generation systems could detect object boundaries using a
473 combination of depth and image-based measures.³⁰ In this case, it may be possible to dynamically
474 adjust the pattern or opacity of overlaid depth information to minimize interference with other
475 visual details. Finally, in its current state, the display brightness is limited and best-suited for
476 indoor environments.

477 Our results also suggest an interesting effect of AR on visual confidence. Visual
478 confidence (i.e., an observers' ability to estimate the reliability of their own perception³¹), might be
479 of particular importance for users who adopt HMD-based tools. While people have extensive
480 experience with which to estimate the reliability of their unaided vision, they have no immediate
481 access to quantitative diagnostics of an HMD. As with other assistive devices, training, practice,
482 or calibration is likely to be necessary in order for users to learn the correct level of visual
483 confidence. Here, we found that accuracy was indeed positively correlated with confidence.
484 However, we also found that when participants used augmented vision, their visual confidence
485 was higher compared to baseline, even when they gave *incorrect* answers. However, it is
486 important to note that this observation was made from a sample of participants with simulated,
487 temporary visual impairments, and thus may not generalize to other populations. Future research
488 will therefore need to explore our understanding of visual confidence in AR.

489 Based on the results and feedback in these studies, several future directions are
490 conceivable. For instance, recent advantages in computer vision could be harnessed to develop
491 "smart" overlays that, for example, are able to highlight flat and uneven surfaces and identify
492 stairs, apertures, or even people. In addition, more sophisticated algorithms to automatically
493 provide simplified and enhanced spatial information could potentially be implemented in real-time

494 AR.^{32, 33} The rapid developments in mobile electronic consumer devices' computing power
495 together with universal platforms for application development, provide vast opportunities to
496 implement and improve visual assistive technology.

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502

References

1. Varma R, Vajaranant TS, Burkemper B, et al. Visual Impairment and Blindness in Adults in the United States: Demographic and Geographic Variations from 2015 to 2050. *JAMA Ophthalmol* 2016;134:802-9.
2. Massof RW. A Systems Model for Low Vision Rehabilitation. II. Measurement of Vision Disabilities. *Optom Vis Sci* 1998;75:349-73.
3. Stelmack JA, Szlyk JP, Stelmack TR, et al. Psychometric Properties of the Veterans Affairs Low-Vision Visual Functioning Questionnaire. *IOVS* 2004;45:3919-28.
4. Massof RW, Rickman DL, Lalle PA. Low-Vision Enhancement System. *J Hopkins APL Tech D* 1994;15:120-5.
5. Moshtael H, Aslam T, Underwood I, Dhillon B. High Tech Aids Low Vision: A Review of Image Processing for the Visually Impaired. *Transl Vis Sci Technol* 2015;4:6.
6. Culham LE, Chabra A, Rubin GS. Clinical Performance of Electronic, Head-Mounted, Low-Vision Devices. *Ophthalmic Physiol Opt* 2004;24:281-90.
7. Peli E, Peli T. Image Enhancement for the Visually Impaired. *Optical Engineering* 1984;23:47-51.
8. Crossland MD, Silva RS, Macedo AF. Smartphone, Tablet Computer and E-Reader Use by People with Vision Impairment. *Ophthalmic Physiol Opt* 2014;34:552-7.
9. Vargas-Martin F, Peli E. Augmented-View for Restricted Visual Field: Multiple Device Implementations. *Optom Vis Sci* 2002;79:715-23.
10. Zhao Y, Hu M, Hashash S, Azenkot S. Understanding Low Vision People's Visual Perception on Commercial Augmented Reality Glasses. *CHI Conference on Human Factors in Computing Systems* 2017:4170-81.
11. Hwang AD, Peli E. An Augmented-Reality Edge Enhancement Application for Google Glass. *Optom Vis Sci* 2014;91:1021-30.

12. Al-Atabany W, Memon MA, Downes SM, Degenaar PA. Designing and Testing Scene Enhancement Algorithms for Patients with Retina Degenerative Disorders. *BioMedical Engineering OnLine* 2010;9:27.
13. Peli E, Goldstein RB, Young GM, et al. Image Enhancement for the Visually Impaired. Simulations and Experimental Results. *IOVS* 1991;32:2337-50.
14. Peli E. Vision Multiplexing: An Engineering Approach to Vision Rehabilitation Device Development. *Optom Vis Sci* 2001;78:304-15.
15. World Health Organization. International Statistical Classification of Diseases and Related Health Problems 10th Edition. In: World Health Organization; 2016.
16. Hicks SL, Wilson I, Muhammed L, et al. A Depth-Based Head-Mounted Visual Display to Aid Navigation in Partially Sighted Individuals. *PLoS One* 2013;8:e67695.
17. Bordier C, Petra J, Dauxerre C, et al. Influence of Background on Image Recognition in Normal Vision and Age-Related Macular Degeneration. *Ophthalmic Physiol Opt* 2011;31:203-15.
18. Everingham M, Thomas B, Troscianko T. Head-Mounted Mobility Aid for Low Vision Using Scene Classification Techniques. *Int J of Virt Reality* 1998;3:1-10.
19. Everingham MR, Thomas BT, Troscianko T. Wearable Mobility Aid for Low Vision Using Scene Classification in a Markov Random Field Model Framework. *International Journal of Human-Computer Interaction* 2003;15:231-44.
20. Peyrin C, Ramanoel S, Roux-Sibilon A, et al. Scene Perception in Age-Related Macular Degeneration: Effect of Spatial Frequencies and Contrast in Residual Vision. *Vision Res* 2017;130:36-47.
21. van Rheede JJ, Wilson IR, Qian RI, et al. Improving Mobility Performance in Low Vision with a Distance-Based Representation of the Visual Scene. *IOVS* 2015;56:4802-9.
22. Wilson IR, Van Rheede JJ, Campbell AM, et al. A Mobile Image Enhancement System for Sight Impaired Individuals. *IOVS* 2016;57.

23. Microsoft. Hololens Hardware Details. https://developer.microsoft.com/en-us/windows/mixed-reality/hololens_hardware_details. Accessed: 07.11.2017.
24. Odell NV, Leske DA, Hatt SR, et al. The Effect of Bangerter Filters on Optotype Acuity, Vernier Acuity, and Contrast Sensitivity. *J AAPOS* 2008;12:555-9.
25. Landis JR, Koch GG. The Measurement of Observer Agreement for Categorical Data. *Biometrics* 1977;33:159-74.
26. R Version 3.3.2: Vienna, Austria: R Foundation for Statistical Computing; 2016. Available at: <https://www.R-project.org>.
27. Derrick B, Russ B, Toher D, White P. Test Statistics for the Comparison of Means for Two Samples That Include Both Paired and Independent Observations. *J Mod Appl Stat Meth* 2017;16:137-57.
28. Bochsler TM, Legge GE, Kallie CS, Gage R. Seeing Steps and Ramps with Simulated Low Acuity: Impact of Texture and Locomotion. *Optom Vis Sci* 2012;89:E1299-307.
29. Kallie CS, Legge GE, Yu D. Identification and Detection of Simple 3d Objects with Severely Blurred Vision. *Invest Ophthalmol Vis Sci* 2012;53:7997-8005.
30. Wang SH, Pan HR, Zhang CY, Tian YL. Rgb-D Image-Based Detection of Stairs, Pedestrian Crosswalks and Traffic Signs. *Journal of Visual Communication and Image Representation* 2014;25:263-72.
31. Mamassian P. Visual Confidence. *Annu Rev Vis Sci* 2016;2:459-81.
32. DeCarlo D, Finkelstein A, Rusinkiewicz S, Santella A. Suggestive Contours for Conveying Shape. *ACM Transactions on Graphics (Proc. SIGGRAPH)* 2003;22:848-55.
33. Rusinkiewicz S, Burns M, DeCarlo D. Exaggerated Shading for Depicting Shape and Detail. In: *ACM Transactions on Graphics*; Boston, MA: Boston, MA. ACM; 2006:1199-205.

Figure legends

Figure 1. HoloLens hardware. **(A)** The HoloLens has binocular see-through displays (red arrows), a sensor bar (blue dashed box), and an onboard computer. **(B)** Users wear HoloLens by tightening an adjustable band around the head and positioning the screen in front of their eyes.

Figure 2. Augmented reality application. **(A,B)** The HoloLens creates a 3D map of the physical environment (A) and can overlay an augmented stereoscopic view (B). The example overlay shows nearby surfaces (less than 2.0 m) as warm colors, and farther surfaces as cool colors (2.0 m and farther). This is the red-to-blue AR used in Experiment 2. **(C)** Several other example views of the same scene demonstrate how the color and intensity can be customized for individual users. These are a subset of the options presented to participants in Experiment 1. All examples were captured from the HoloLens using the scene camera positioned between the user's eyes.

Figure 3. Example tasks. **(A)** Images of the five objects. To decrease the probability of getting the correct answer based purely on the approximate size of the object, several objects were selected to have a similar shape and size. **(B)** Example of one of the three unique room layouts used in the mobility task for Experiment 2. Layouts were comprised of a set of tables and chairs in different locations, with different objects placed on the tables as well.

Figure 4. Experiment 1 results. Results are shown for person localization **(A)**, pose recognition **(B)**, object recognition **(C)** and mobility **(D)** tasks. Bar heights in A-C indicate percent correct (left column) and average confidence (right column) of each participant across baseline and AR trial blocks. Bar heights in D indicate mean distance each participant stopped in front of the obstacle in the two trial blocks. On the last AR trial, Participant 4 changed direction and walked towards a wall. He detected the wall visually using the AR color before hitting it with his cane, so this distance was recorded and used for analysis. Error bars in confidence ratings and mobility task indicate standard error. AR = Augmented Reality; p1-4 = Participants 1-4.

Figure 5. Experiment 2 results for visual identification tasks in terms of percent correct **(A, B, C)** and confidence ratings **(D, E, F)**. Bar heights indicate the mean across participants within each group (control, color, opacity), and error bars indicate standard error. Results for each group are summarized with two

bars that represent data from the first (baseline) and second (AR) block of trials. AR = Augmented Reality. *** $P < .001$; * $P < .05$.

Figure 6. Relationship between performance and confidence. Mean confidence ratings are shown separately for correct/incorrect trials in pose (A), object (B), and gesture (C) recognition. Data are plotted as in Figure 4, except the two test conditions (color and opacity) are combined. AR = Augmented Reality. Partially overlapping t-tests were used to compare means between binned data. T-statistics (degrees of freedom) for significant differences: Pose recognition, correct trials, test condition: $T(121.7)=3.08$; Object recognition, correct trials, test condition: $T(112.15)=4.81$; Object recognition, incorrect trials, test condition: $T(144.26)=5.49$; Gesture recognition, correct trials, test condition (unpaired t-test): $T(17) = 3.69$; Gesture recognition, incorrect trials, test condition: $T(144.26)=-5.49$. *** $P < .001$; ** $P < .01$, * $P < .05$.

Figure 7. Experiment 2 mobility task results. Differences in subjective responses compared to baseline in the control group and test groups are shown for risk of collision (A) and usefulness of vision (B). Positive values indicate ratings higher than baseline, and the maximum absolute difference is 6. Error bars indicate standard error. AR = Augmented Reality. *** $P < .001$; ** $P < .01$.