

1 **Postprandial administration but not controlled release in the colon increases**
2 **oral bioavailability of DF030263, a promising drug candidate for chronic**
3 **lymphocytic leukemia**

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30 **ABSTRACT**

31 For treatment of chronic cancers, the oral administration route is preferred as it provides
32 numerous advantages over other delivery routes. However, these benefits of oral chemotherapy
33 can be limited due to unfavorable pharmacokinetics. Accordingly, pharmacokinetic
34 development of chemotherapeutic agents is crucial to the improvement of cancer treatment. In
35 this study, assessment and optimization of biopharmaceutical properties of a promising drug
36 candidate for cyclin-dependent kinase 9 (CDK9) inhibitor (DF030263) was performed to
37 promote oral delivery. Oral bioavailability of DF030263 in fasted rats was 23.8%, and a distinct
38 double-peak phenomenon was observed. A two-site absorption windows mechanism was
39 proposed as a possible explanation to the phenomenon. The two-site absorption window
40 hypothesis was supported by *in vitro* solubility assays in biorelevant fluids with different pH
41 levels, as well as by *in silico* simulation by GastroPlus™. Controlled release to the colon was
42 conducted in rats in order to exploit the colonic absorption window but did not improve the
43 oral bioavailability. On the other hand, oral administration at postprandial conditions in rats
44 (performed based on the high *in vitro* solubility in fed state simulated fluid and reduced pH-
45 dependency) resulted in an almost 3-fold increase in bioavailability to 63.6%. In conclusion,
46 this study demonstrates an efficient *in vitro-in vivo-in silico* drug development approach for
47 improving the oral bioavailability of DF030263, a promising candidate for the treatment of
48 chronic lymphocytic leukemia.

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1. Introduction

Treatment of cancer is often limited by lack of efficacy and serious adverse effects. Unsatisfactory efficacy in many cases is related to unfavorable pharmacokinetics and biodistribution profiles including poor bioavailability, rapid clearance and limited distribution to the tumor tissues [1]. The key aspect of this is that sufficient drug concentration has to be achieved and maintained at the site of action for the optimal anticancer efficacy [2]. Therefore, along with the development of targeted anticancer therapies by means of well-defined molecular targets or biologic signaling streams, pharmacokinetic development and optimization of chemotherapeutic agents are important to improve the treatment outcomes of cancer [3].

While the majority of chemotherapy regimens in cancer depends on parenteral delivery, oral administration of anticancer agents is desired for several reasons. Oral dosing allows self-administration by the patients and avoids the inconvenience of intravenous injections which needs hospitalization [4, 5]. Therefore, it improves patient compliance and reduces costs of therapy. It also prevents risk of infection that might be caused as a complication of injectable routes of administration. Most importantly, it makes treatment of chronic diseases more practical [5, 6]. However, many anticancer agents possess unfavorable properties that make sufficient systemic exposure following oral administration challenging. These properties are mainly physicochemical characteristics that result in low solubility, poor permeability, high efflux and rapid pre-systemic metabolism [2].

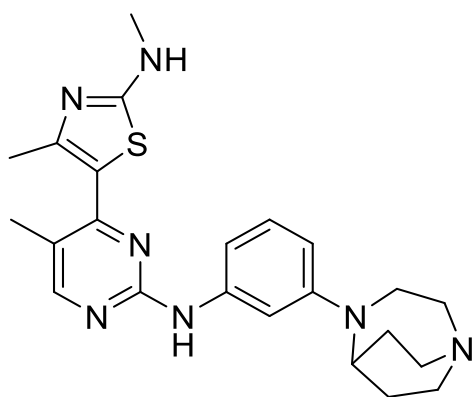
Cyclin-dependent kinases (CDKs) are essential in cell growth as they control progression of cell cycles and regulate transcription [7]. CDK inhibitors have been discovered and developed on this premise to seek inhibition of unsuppressed cancer cell proliferation [7, 8]. Among the

77 CDK family, CDK9 is particularly related to the regulation of RNA transcription. High
78 expression of CDK9 and cyclin T1, corresponding cyclin partner of CDK9, was observed in
79 chronic lymphocytic leukemia (CLL), indicating their key roles in pathologic mechanism of
80 the disease [8-10]. We have recently reported a series of highly active and selective inhibitors
81 of CDK9 as candidates for the treatment of CLL. Among the candidates, DF030263 was one
82 of the most efficacious and selective compounds *in vitro* [11].
83 Therefore, the aim of this work was to assess and to optimize the biopharmaceutical properties
84 of DF030263 in order to achieve efficient treatment of CLL following oral administration of
85 this compound. An *in vitro-in vivo-in silico* approach was applied to provide adequate solution
86 towards improvement of the oral bioavailability. Biopharmaceutical optimization approaches
87 including controlled release in the colon and postprandial conditions have also been assessed
88 in this work.

90 **2. Material and methods**

91 **2.1. Materials**

92 DF030263 (5-(2-((3-(1,4-diazabicyclo[3.2.2]nonan-4-yl)phenyl)amino)-5-methylpyrimidin-4-
93 yl)-N,4-dimethylthiazol-2-amine, Figure 1) was synthesized in School of Pharmacy, University
94 of Nottingham (Nottingham, UK) as reported as compound **30m** in our previous publication
95 [11]. Sodium taurocholate (NaTc), NaCl, NaOH (pellets), NaH₂PO₄, glacial acetic acid,
96 lecithin, chlorpromazine and dexamethasone were obtained from Sigma (Gillingham, UK). Rat
97 plasma was purchased from Sera Laboratories International (West Sussex, UK). Polyethylene
98 glycol (PEG) 400 and all solvents (HPLC grade or higher) were obtained from Fisher Scientific
99 (Leicestershire, UK). All other chemicals were analytical reagent grade or higher.



100
101 **Figure 1.** Chemical structure of DF030263 [11].

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103 **2.2. *In vitro* solubility assay**

104 **2.2.1. Preparation of simulated fluids**

105 Three different types of fluids simulating the gastrointestinal environment were prepared
106 according to previously reported preparation methods [12-14]: fasted state simulated gastric
107 fluid (FaSSGF), fasted state simulated intestinal fluid (FaSSIF) and fed state simulated
108 intestinal fluid (FeSSIF). The composition of these three simulated fluids were as described in
109 Table 1. Prior to the assay, the pH of FaSSGF was adjusted to 1.6 and 3.0 using HCl and the
110 pH of FaSSIF and FeSSIF was adjusted to be between 5.0-7.8 with interval of 0.2 using HCl
111 or NaOH. All fluids were prepared on the day before the assay and stored at 4°C until use.

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113 **Table 1. Composition of the simulated fluids (mM)**

	FaSSGF	FaSSIF	FeSSIF
NaTc	0.08	3	15
Lecithin	0.02	0.75	3.75
NaCl	34.2	105.9	203.3
NaOH	-	8.7	102
NaH₂PO₄	-	8.2	-
Acetic acid	-	-	144

114 FaSSGF, fasted state simulated gastric fluid; FaSSIF, fasted state simulated intestinal fluid; FeSSIF, fed state
115 simulated intestinal fluid.

117 **2.2.2. Solubility assay**

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2 118 On the day of assay, 198 μL of test medium (FaSSGF, FaSSIF, FeSSIF and water) was
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5 119 aliquoted into centrifugal tubes (Costar Spin-X Centrifuge Tube, Fisher Scientific,
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7 120 Leicestershire, UK). A volume of 2 μL of 20 mM stock solution in DMSO was then spiked
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9 121 into each tube to yield 200 μM of test concentration. The tubes were incubated at 37°C shaking
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12 122 at 250 rpm for 2 h using a shaking incubator (Thermo Scientific MaxQ4000, Thermo Scientific,
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14 123 OH, USA). After the incubation, the samples were immediately centrifuged for 5 min at 2400
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17 124 g (Heraeus Fresco 17 Centrifuge, Thermo Electron, MA, USA). The filtrate was collected and
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19 125 subjected to analysis as described below. The assay was performed in triplicate.
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24 127 **2.2.3. Sample analysis**

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26 128 To 50 μL of sample, 10 μL of internal standard stock solution (100 μM dexamethasone, 50%
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29 129 acetonitrile in water) was spiked. For FaSSGF samples, 200 μL of 1 M NaOH was added and
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31 130 for FaSSIF, FeSSIF and water samples, 200 μL of 0.1 M NaOH was added. Two mL of methyl-
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34 131 tert-butyl ether was then added and the mixture was vortex-mixed for 10 min and centrifuged
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36 132 at 1160 g for 10 min. The organic layer was transferred and evaporated to dryness under N_2
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39 133 gas at 40°C. Hundred μL of 40% acetonitrile in water was then added for reconstitution and
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41 134 vortex-mixed for 10 min before being transferred to HPLC vial for analysis.
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46 136 The prepared samples were analyzed by a HPLC-UV system consisting of a Waters 600 Pump,
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49 137 Waters 717 Autosampler and Waters 2996 Photodiode Array Detector. A separate column oven
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51 138 was used to maintain the column temperature at 40°C. The stationary phase was a Gemini C18
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53 139 250 \times 4.6 mm, 5 μm particle size equipped with a SecurityGuard 2 \times 4 mm, 3 μm particle size
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56 140 (Phenomenex, Macclesfield, UK). Mobile phase was a mixture of acetonitrile and 10 mM
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58 141 ammonium acetate buffer with pH adjusted to 5.0 with glacial acetic acid (40:60, v/v). The
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142 flow rate was 0.5 mL/min and 60 μ L was injected. Chromatograms were observed at 256.5 nm
1 of UV wavelength.

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145 **2.3. *In vivo* pharmacokinetic experiment**

146 **2.3.1. Animals**

147 This study was conducted in accordance with an approved protocol by the Institutional Animal
148 Use and Care Committee at Rutgers, The State University of New Jersey (#16-001). Male
149 Sprague Dawley rats (Envigo, Inc., Indianapolis, IN) weighing 300-350 g were used for the
150 experiment. Animals were housed at controlled temperature, 12 h light/dark cycle and with free
151 access to food and water. The acclimatization of the animals was at least for four days. Surgical
152 procedures were performed under general anesthesia induced by inhalation of isoflurane with
153 an air carrier (3% for induction and <3% for maintenance). All rats underwent right jugular
154 vein cannulation for blood sampling. For the group that received colonic administration,
155 cannulation of the cecum was performed based on a previously reported protocol [15].
156 Laparotomy was performed to gain access to the large intestine. A small hole in the cecum was
157 made with a 19 G needle and the cannula (built using PE-50 tubing) was inserted. Animals
158 were allowed to recover for two days and were fasted up to 12 h before the pharmacokinetic
159 experiment (except postprandial conditions experiment) with free access to drinking water.

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161 **2.3.2. Pharmacokinetic experiments**

162 Formulations of DF030263 were prepared in PEG400:water (50:50, v/v) in concentrations of
163 2 or 4 mg/mL. For intravenous administration, formulation of 2 mg/mL was delivered at 1
164 mL/kg via the jugular vein cannula followed by 0.3 mL of heparinized saline (50 IU/mL) to
165 ensure complete administration. Oral administration was conducted with the formulation of 4
166 mg/mL at 3 mL/kg using an oral gavage tube. Colonic administration was also performed with

167 the formulation of 4 mg/mL at 3 mL/kg delivered via the cannula inserted into the cecum. The
168 formulation was infused using a syringe pump (PHD Ultra, Harvard Apparatus, Holliston, MA,
169 USA) at a constant rate for 1 h for colonic administration. Following the administration, blood
170 samples (250 μ L) were collected from the jugular vein cannula at pre-determined time points.
171 Blood samples were centrifuged (3000 g, 10 min) and plasma samples were stored in -80°C
172 until analysis.

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174 2.3.3. Sample analysis

175 A volume of 100 μ L of plasma was used for sample preparation procedure. The plasma samples
176 were spiked with 10 μ L of internal standard stock solution (5 μ g/mL chlorpromazine, 50%
177 acetonitrile in water). Three hundred μ L of 0.1 M NaOH and 2 mL of methyl-tert-butyl ether
178 were then added. The mixture was vortex-mixed for 1 min and centrifuged at 1160 g for 10
179 min. The supernatant organic layer was transferred to new glass tubes and evaporated to
180 dryness under gentle stream of N₂ gas at 40°C. Hundred μ L of 40% acetonitrile in water was
181 added to dried samples for reconstitution and vortex-mixed for 30 s before being transferred to
182 HPLC vial for analysis.

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184 The HPLC-UV system was composed of Agilent 1260 Infinity equipped with quaternary pump,
185 high performance autosampler, thermostated column compartment and diode array detector.
186 The stationary phase was a Gemini C18 250 \times 4.6 mm, 5 μ m particle size equipped with a
187 SecurityGuard 2 \times 4 mm, 3 μ m particle size (Phenomenex, Macclesfield, UK) and the column
188 temperature was maintained at 40°C. Mobile phase was a mixture of acetonitrile, methanol and
189 10 mM ammonium acetate buffer with pH adjusted to 5.0 with glacial acetic acid (30:20:50,
190 v/v). The flow rate was 0.4 mL/min and 80 μ L was injected. Chromatograms were observed at
191 256.5 nm of UV wavelength.

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2 193 Sample stability was tested prior to the pharmacokinetic experiment to ensure sample integrity
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5 194 during sample storage and analysis. Samples of rat plasma (n = 4) spiked with low (25 ng/mL)
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7 195 and high (8 µg/mL) quality control concentrations were prepared and stored at the following
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10 196 conditions: 4 h at room temperature to test bench-top stability; 1, 2 and 4 weeks at -80°C to
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12 197 test storage condition stability. Autosampler stability was tested at the same concentrations
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14 198 with processed samples stored at 5°C for 24 h. All stability results were within ±15% relative
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17 199 error. Accordingly, all sample storage and preparation were performed within the limit of
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19 200 stability tested.
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24 202 **2.4. Deconvolution of plasma concentration-time profiles**

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26 203 Deconvolution of plasma concentration-time profiles was conducted using Phoenix WinNonlin
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29 204 version 6.3 (Certara, Princeton, NJ, USA). The mean plasma concentration-time profiles
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31 205 following oral and intravenous administrations were used for the deconvolution. The results of
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33
34 206 deconvolution were expressed as cumulative input vs time and input rate vs time.
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39 208 **2.5. *In silico* simulation of absorption sites**

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41 209 Intestinal absorption of DF030263 compound in different compartments of the gastrointestinal
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44 210 tract was simulated *in silico* using GastroPlus™ version 9.0.0007 with built-in ADMET
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46 211 Predictor™ version 7.2.0.0 module (Simulations Plus, Inc., Lancaster, CA, USA). The input
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49 212 parameters are listed in Table 2. Parameters and settings not mentioned in the Table 2 were
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51 213 used as predicted by the ADMET Predictor™ or as given by software default. The physiology
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54 214 setting was selected as “Rat-Fasted” or “Rat-Fed” and paracellular permeation option was
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56 215 turned on. Percentages of the dose absorbed at different compartments of the gastrointestinal
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58 216 tract were simulated at both fasted and fed states for rats.
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218 **Table 2. Input parameters for *in silico* simulation of intestinal absorption of DF030263**

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219 **compound using GastroPlus™**

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Parameters	Value
Molecular weight (g/mol)	435.6
Log P	3.1
pK _a	10.7
Human jejunal permeability ($\times 10^{-4}$ cm/s)	1.37 ^a
Diffusion coefficient ($\times 10^{-5}$ cm ² /s)	0.6288 ^a
Drug particle density (g/mL)	1.2 ^b
Mean precipitation time (sec)	900 ^b
Reference solubility (mg/mL)	0.03846 ^c
Biorelevant solubilities (mg/mL)	
FaSSGF (pH 1.6)	0.6737 ^c
FaSSIF (pH 6.6)	0.04935 ^c
FeSSIF (pH 5.0)	0.06529 ^c

^a Predicted by GastroPlus™

^b GastroPlus™ default values

^c Experimental results

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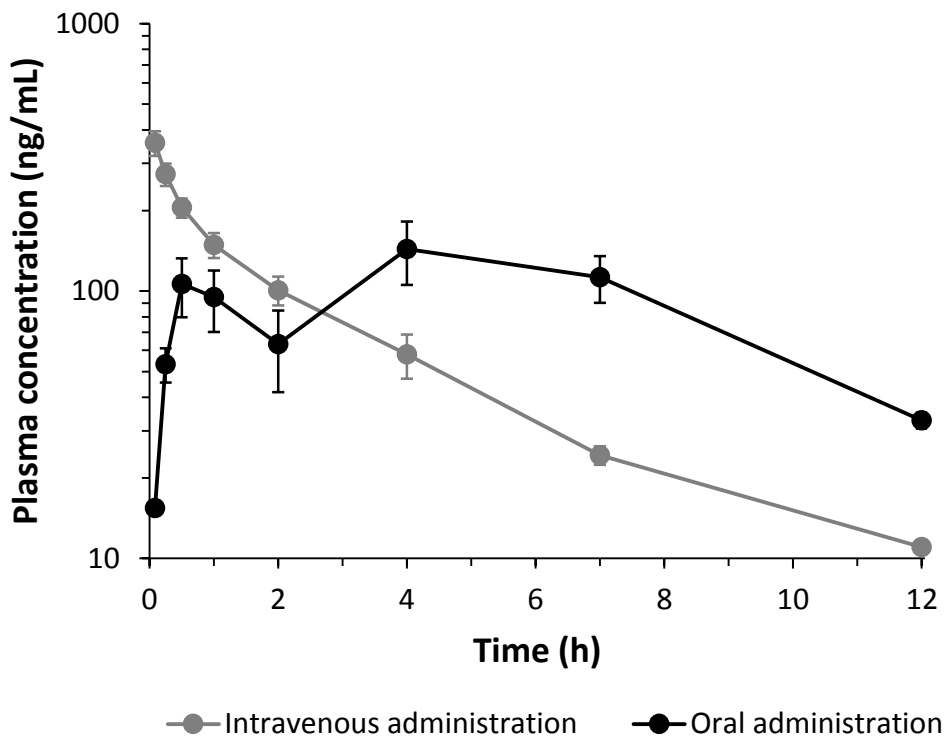
2.6. Statistical analysis

Data were expressed as mean \pm standard error of the mean (SEM). Statistical significance of differences between two groups was determined by two-tailed unpaired t-test. A *p*-value of less than 0.05 was defined as statistically significant. Statistical analysis was performed using GraphPad Prism version 7.01 (GraphPad Software, Inc., La Jolla, CA, USA). Plasma pharmacokinetic parameters were obtained by non-compartmental analysis using Phoenix WinNonlin 6.3 software (Certara, Princeton, NJ, USA).

3. Results

3.1. *In vivo* oral bioavailability evaluation of DF030263

234 *In vivo* oral bioavailability of DF030263 was evaluated in rats and the mean plasma
235 concentration-time profiles are shown in Figure 2. The plasma concentration-time profile
236 obtained following oral administration showed a distinct double-peak phenomenon, which was
237 not apparent following intravenous administration. The first peak appeared after rapid
238 absorption of the compound at 0.5 h while the second peak followed a delayed absorption,
239 appearing at 4 h. Although the time between the two peaks varied for individual animals, this
240 double-peak phenomenon was observed in all rats tested for oral administration (n = 4). The
241 mean oral bioavailability of DF030263 was determined to be 23.8% and other pharmacokinetic
242 parameters obtained from the plasma concentration-time profiles are shown in Table 3.



243
244 **Figure 2.** Mean plasma concentration-time profiles of DF030263 in rats following intravenous
245 (2 mg/kg) and oral (12 mg/kg) administration (n = 4, each group).

248 **Table 3.** Plasma pharmacokinetic parameters obtained from *in vivo* pharmacokinetic
 249 experiments

<i>Parameters</i>	Intravenous administration (n = 4)	Oral administration at fasted state (n = 4)	Oral administration at fed state (n = 6)	Colonic administration (n = 3)*
Dose (mg/kg)	2	12	12	12
C₀ (ng/mL)	410.8 ± 46.4	-	-	-
C_{max} (ng/mL)	-	149.9 ± 34.8	346.6 ± 50.3**	302.2 ± 37.1
T_{max} (h)	-	4	7	1.5
CL (L/h/kg)	2.9 ± 0.4	-	-	-
V_{ss} (L/kg)	9.9 ± 1.1	-	-	-
AUC_{0→t} (h·ng/mL)	673.1 ± 98.1	960.9 ± 231.2	2570.2 ± 382.4**	978.9 ± 143.8
Bioavailability (%)	-	23.8 ± 5.7	63.6 ± 9.5**	24.2 ± 3.6

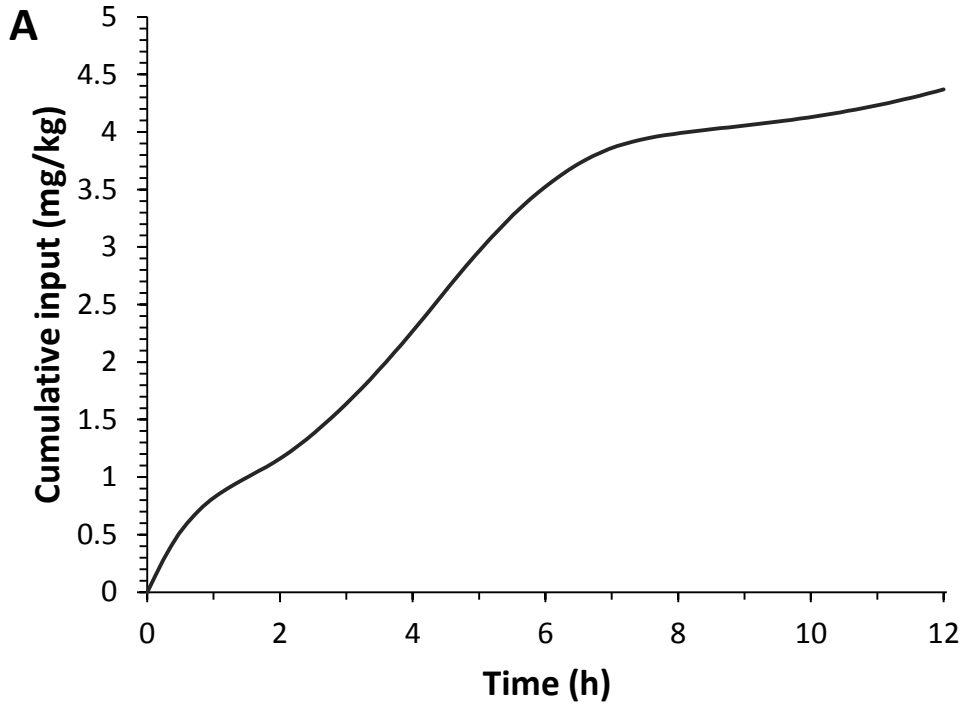
* Colonic administration was performed by infusion for 1 h through a cannula inserted to the cecum.

** Significantly different compared to oral administration at fasted state ($p < 0.05$).

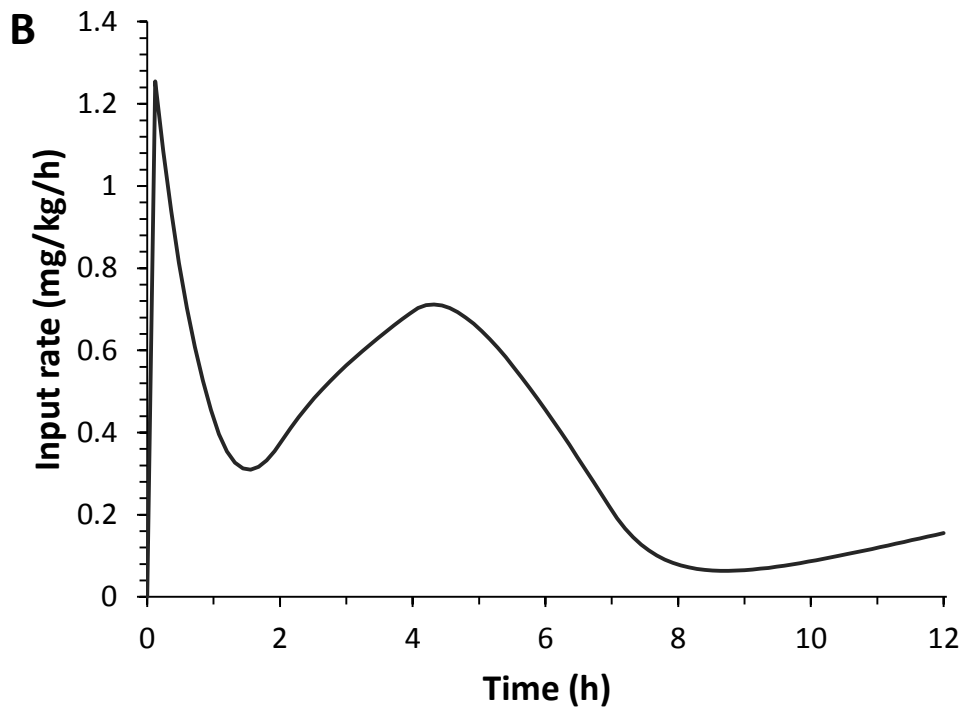
C₀, concentration extrapolated to time zero; C_{max}, maximum concentration observed; T_{max}, time of maximum concentration observed; t_{1/2}, elimination half-life; CL, clearance; V_{ss}, volume of distribution at steady state; AUC_{0→t}, area under the curve from time zero to the last observed point.

3.2. Deconvolution of plasma concentration-time profiles

Deconvolution of the plasma concentration-time profiles obtained from *in vivo* oral bioavailability evaluation was performed in order to understand the absorption or input function of DF030263 following oral administration. The results of cumulative input or input rate vs time are shown in Figure 3. It can be seen from Figure 3A that the absorption shows a biphasic input function; the first phase between 0-1 h and the second phase between 2-6 h. This becomes more apparent in Figure 3B where two peaks are shown from the input rate vs time graph. These results indicated possibility of existence of two absorption windows for DF030263 along the gastrointestinal tract.



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52 267 **Figure 3.** Deconvolution results of plasma concentration-time profiles obtained from oral
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54 268 bioavailability evaluation of DF030263. **A**, cumulative input vs time; **B**, input rate vs time.
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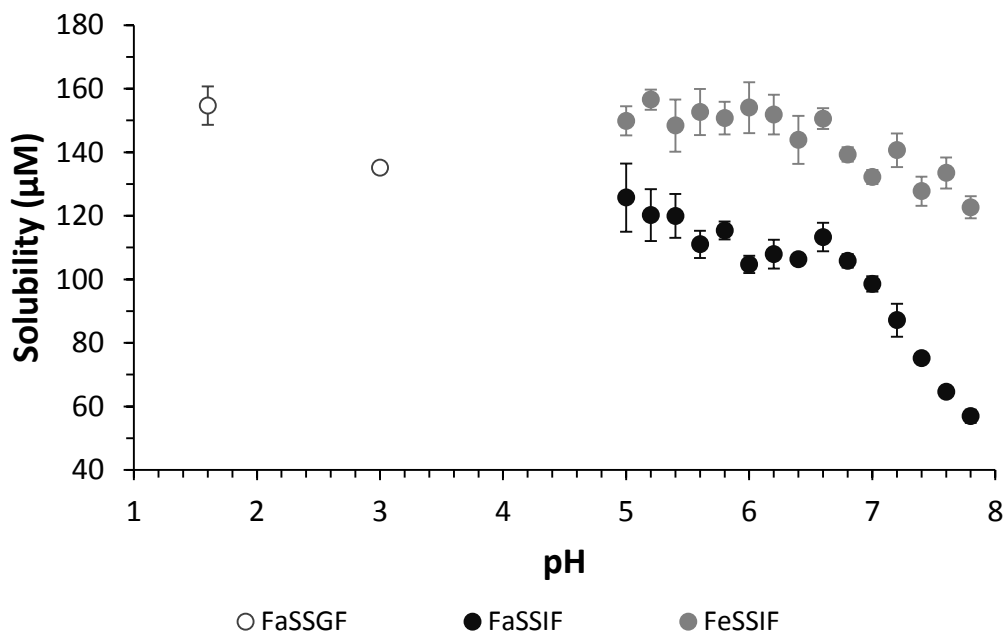
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271 **3.3. *In vitro* solubility tests**

272 *In vitro* solubility tests were conducted with simulated fluids of FaSSGF, FaSSIF and FeSSIF
273 to provide information on solubilization behavior of DF030263 along the gastrointestinal tract.
274 The pH values of these simulated fluids are commonly used to represent the mean pH found in
275 the gastrointestinal tract. However, different pH values are observed in different segments of
276 the gastrointestinal tract *in vivo* [16-18]. Therefore, in this study, the pH of each simulated fluid
277 was adjusted to represent the pH range found *in vivo* and solubility of DF030263 was tested at
278 each pH level. In general, DF030263 showed higher solubility in acidic environment (Figure
279 4). DF030263 exhibited pH-dependent solubility especially in FaSSIF where the solubility
280 decreased steeply when the pH increased above 6.6. This indicated that there could be high
281 probability of precipitation in segments of gastrointestinal tract with higher pH levels. This pH-
282 dependent decrease was less apparent in FeSSIF. Solubility in water was $88.3 \pm 2.6 \mu\text{M}$.

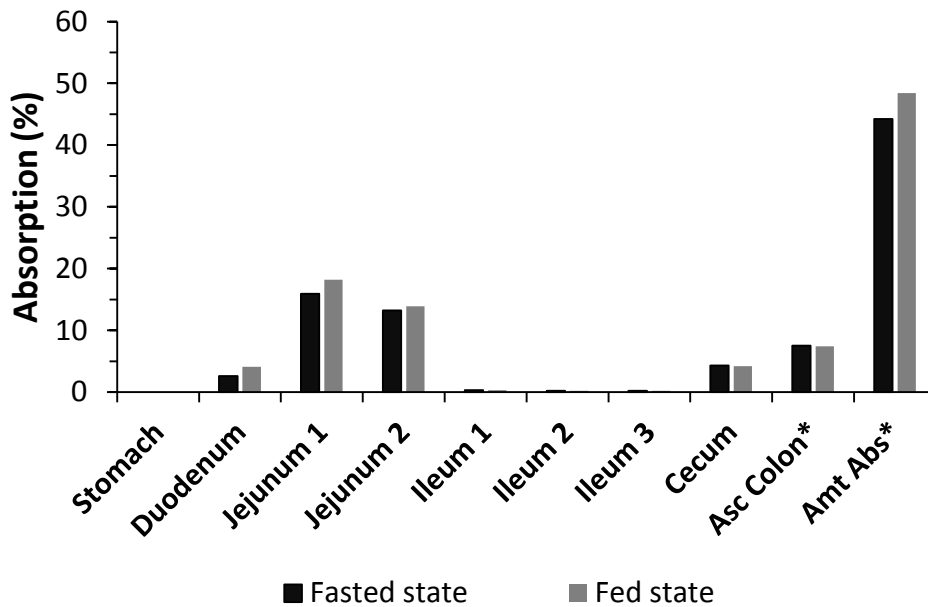


283 **Figure 4.** Solubility of DF030263 in FaSSGF, FaSSIF and FeSSIF at various pH (n = 3).
284 FaSSGF, fasted state simulated gastric fluid; FaSSIF, fasted state simulated intestinal fluid;
285 FeSSIF, fed state simulated intestinal fluid.

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288 **3.4. *In silico* simulation of intestinal absorption**

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2 289 *In silico* simulation was performed to predict intestinal absorption of DF030263 *in vivo*.
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5 290 GastroPlus™ utilizes advanced compartmental absorption and transit (ACAT) model for their
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7 291 intestinal absorption simulation [19], which compartmentalizes the gastrointestinal tract into
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10 292 nine different compartments. Therefore it was able to predict the fraction of the dose that will
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12 293 be absorbed at the different compartments. The simulation results at both fasted and fed states
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14 294 of the rat are shown in Figure 5. The results show that DF030263 is predicted to be firstly
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16 295 absorbed at the proximal regions of the small intestine and then has an additional absorption
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19 296 window in the cecum and colon.

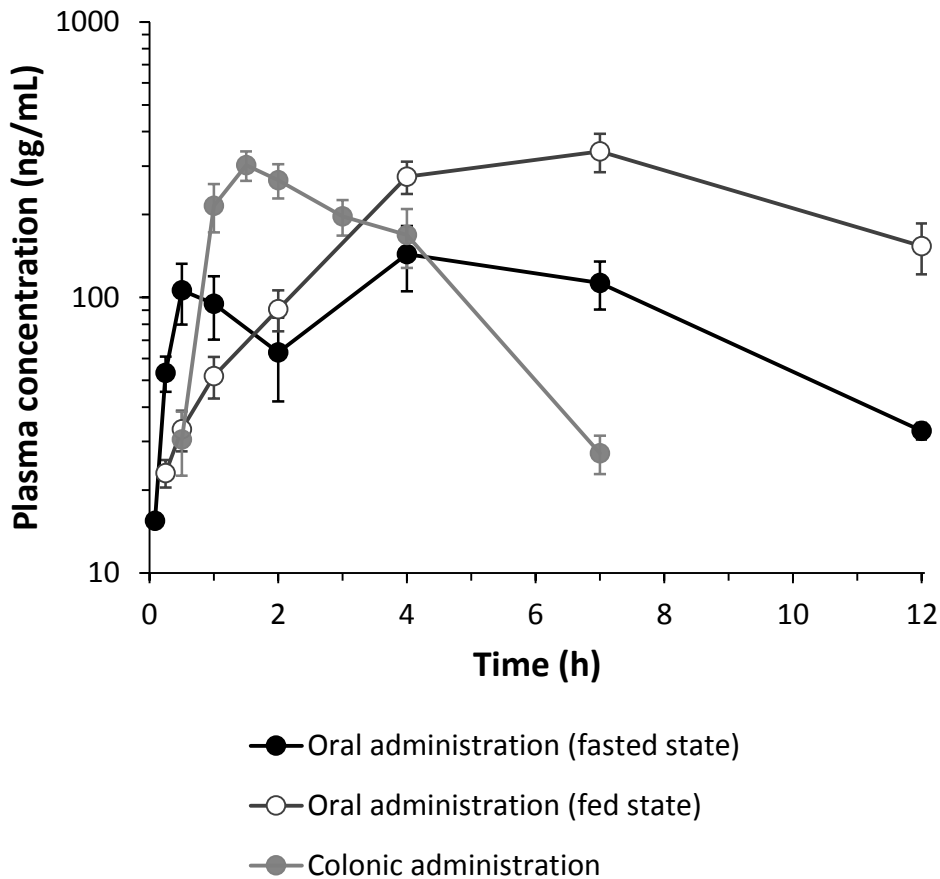


297
298 **Figure 5.** *In silico* simulation of intestinal absorption of DF030263 at each compartment of the
299 gastrointestinal tract. *Asc Colon, ascending colon; Amt Abs, total amount absorbed in the
300 gastrointestinal tract.

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302 **3.5. Colonic and postprandial administration of DF030263**

303 Following the above results, colonic and postprandial administration of DF030263 were
304 evaluated in order to improve oral bioavailability of DF030263. Colonic administration was

305 delivered by infusion through the cannula inserted to the cecum for 1 h to mimic controlled
306 release of the drug in the large intestine. Postprandial oral gavage administration was
307 performed on rats that had free access to food and water throughout the experiment. The
308 double-peak phenomenon observed after administration by oral gavage at fasted state was not
309 seen in the case of postprandial administration or colonic delivery (Figure 6). Colonic
310 administration resulted in rapid absorption ($T_{max} = 1.5$ h) but no improvement in bioavailability
311 was noted (Table 3). On the other hand, oral administration at fed state resulted in significantly
312 higher C_{max} and bioavailability compared to fasted state.



313
314 **Figure 6.** Mean plasma concentration-time profiles of DF030263 in rats following oral
315 administration at fed state (12 mg/kg, n = 6) and colonic administration (12 mg/kg, n = 3).

319 **4. Discussion**

320 **4.1. *In vivo* oral bioavailability evaluation and the double-peak phenomenon**

321 In the initial *in vivo* oral bioavailability evaluation, DF030263 showed mean oral
322 bioavailability of 23.8%. Interestingly, a distinct double-peak phenomenon was observed and
323 it only appeared after oral administration of DF030263 (Figure 2). Similar double-peak
324 phenomenon following oral administration has been reported for a number of drugs including
325 acetaminophen [20], alprazolam [21], cimetidine [22], epinastine [23], furosemide [24],
326 pafenolol [25], ranitidine [26] and veralipride [27]. This phenomenon is usually attributed to
327 the following three main causes [21, 26, 28-31]: 1) enterohepatic recirculation where the drug
328 in the systemic circulation is secreted via bile and reabsorbed from the gastrointestinal tract; 2)
329 variable absorption properties along the gastrointestinal tract (also called “absorption
330 windows”); 3) gastric emptying time is varied depending on motility of the gastrointestinal
331 tract, gastric pH or the lipidic formulation effect. In all cases, this erratic pattern of absorption
332 can potentially be problematic for CDK9 inhibitors as relatively narrow therapeutic window
333 is known to be one of their potential drawbacks [32].

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335 In the case of DF030263 compound, enterohepatic recirculation was excluded from the
336 possible reasons because the plasma concentration-time profile following intravenous
337 administration did not show a double peak. Variance in gastric emptying time was also unlikely
338 to be the reason because the time between the two peaks was as long as 3-6.5 h. Moreover, all
339 four rats orally administered at fasted state displayed double-peaks. Therefore, absorption
340 window of DF030263 in the gastrointestinal tract was thought to be discontinuous and further
341 studies were conducted to elaborate the two-site absorption windows hypothesis.

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4.2. Two-site absorption windows hypothesis

Deconvolution of the plasma concentration-time profiles were conducted to elucidate absorption rate over time for DF030263 following oral administration. Deconvolution represents a mathematical process that can inversely uncover the input function when the oral administration profile is known and drug disposition characteristics are defined by the intravenous administration profile [33]. This allows determination of the absorption characteristics which can often be challenging to measure or quantify *in situ* [34]. As shown in Figure 3, the absorption function of DF030263 exhibited a biphasic process which leads to the two-site absorption.

The two-site absorption windows hypothesis was further supported with the results of the *in silico* simulation using GastroPlus™. The built-in ACAT and generic physiologically-based pharmacokinetic models in the software provide effective predictions of pharmacokinetic profiles in preclinical species and humans [35-38]. In this study, intestinal absorption of DF030263 in different compartments of the rat gastrointestinal tract was predicted. The simulation results predicted clear discontinuation of absorption in the distal region of the small intestine and a second absorption window in the large intestine (Figure 5). Additionally, the secondary absorption phase following oral administration also corresponded to the oral-to-cecal transit time in rats (2-3 h) [25, 39]. This corroborated the assumption that a second absorption window exists in the large intestine. Such site-specific absorption of drugs is known to occur due to properties related to solubility, stability or interaction with luminal contents [40].

The luminal pH levels can differ in different segments of the gastrointestinal tract and therefore *in vitro* solubility tests were carried out in a range of pH using simulated biorelevant media of

369 FaSSGF, FaSSIF and FeSSIF. The solubility of DF030263 was maintained at the highest levels
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2 370 in the acidic environment of FaSSGF and the lower pH ranges of FaSSIF and FeSSIF (Figure
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4 371 4). This is explained by the fact that DF030263 is a weak base with a pK_a of 10.7 (predicted by
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7 372 ACD/Labs, Toronto, Canada) and therefore would be solubilized more efficiently in such
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9 373 acidic environment. When the pH level was increased above 6.6, DF030263 showed pH-
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12 374 dependent solubility with decreasing solubility especially in the FaSSIF. This suggested that
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14 375 DF030263 could be precipitating in the regions of the gastrointestinal tract where the pH is
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16 376 relatively high, such as the distal small intestine. The luminal pH in the rat small intestine
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19 377 increases as it reaches the distal region; from pH 6.5 in the duodenum to 7.1 in the ileum [16].
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22 378 This possibility of precipitation in the small intestine with higher pH has been acknowledged
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24 379 especially for weakly basic compounds and it has been put forward as a critical drug
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26 380 development obstacle, significantly limiting the oral bioavailability of these compounds [41].
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29 381 The luminal pH drops again when it reaches the colon to 6.6 [16], which can provide
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32 382 opportunity for DF030263 to resolubilize and be available for absorption again. The pH-
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34 383 dependent solubility was therefore thought to be the main reason behind the two-site absorption
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36 384 windows. Since humans have a similar luminal pH levels pattern to rats, this phenomenon is
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39 385 likely to occur in humans as well [18].
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44 387 **4.3. Exploitation of the two-site absorption windows**

46 388 In order to improve the oral bioavailability of DF030263, the pH-dependent solubility and
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48 389 potential precipitation in the distal region of the small intestine had to be mitigated. Colonic
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51 390 administration mimicking controlled release of DF030263 in the large intestine and
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53 391 postprandial oral administration were tested for this purpose. Deconvolution and *in silico*
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56 392 simulation of the intestinal absorption both indicated a second absorption window in the large
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58 393 intestine. Additionally, when partial area under the curve (AUC) is calculated for the oral
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1 394 administration profile at fasted state, the window between 2-12 h accounts for 86% of the total
2 395 AUC. With all the above-mentioned factors, colonic administration was thought to possibly
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4 396 improve the bioavailability of DF030263.
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9 398 Colonic administration was performed via a cannula inserted into the cecum and DF030263
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11 399 solubilized in the dosing vehicle was infused for 1 h. Therefore it would not pass through the
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13 400 distal region of the small intestine where the pH is relatively higher and the solubility of
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15 401 DF030263 is lower. Consequently, potential loss in absorption of DF030263 due to the
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17 402 precipitation-resolubilization process can be avoided.
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24 404 As shown in Figure 6, colonic administration resulted in rapid absorption and only single peaks
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26 405 were observed in all rats tested. This is consistent with a previous study where pafenolol, which
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28 406 had double-peak following oral administration, showed a single peak when administered
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30 407 through an intrainestinal cannula to target a specific absorption window in the gastrointestinal
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32 408 tract [25]. In spite of the single peak, colonic delivery did not improve the bioavailability of
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34 409 DF030263, but it was rather comparable to the oral administration at fasted state (Table 3). As
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36 410 a result, it was confirmed that the large intestine is indeed an absorption window but oral
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38 411 bioavailability cannot be improved by controlled release to this site. It is likely that the amount
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40 412 of dose that can be absorbed from the large intestine has been already absorbed from simple
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42 413 oral administration.
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51 415 Postprandial oral administration was also tested mainly based on the premise that solubility is
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53 416 enhanced in fed conditions. The *in vitro* solubility results in Figure 4 clearly show that in
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55 417 FeSSIF, the solubility was higher and was less dependent on the change of pH. The presence
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57 418 of food in the gastrointestinal tract modifies the luminal contents which leads to changes in pH,
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1 419 buffer capacity and surface tension thereby affecting solubilization of drugs [41]. Therefore
2 420 less precipitation of drugs can be anticipated at fed state especially for weak bases with poor
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4 421 solubility [41] which means that more drug can be available for absorption. Also an important
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7 422 food-effect is the delay in gastric emptying which alters the gastrointestinal transit time [40].
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10 423 This delay can allow the drug to reside longer time at the first absorption window which is the
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12 424 proximal region of the small intestine (Figure 5).

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17 426 The plasma concentration-time profile following postprandial oral administration showed a
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19 427 single-peak with substantially improved bioavailability (Figure 6 and Table 3). Avoidance of
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22 428 the double-peak phenomenon by the food-effect has been previously reported [31, 39] but did
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24 429 not necessarily relate to increase in bioavailability. In the case of DF030263, higher solubility,
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27 430 less precipitation and prolonged exposure to the first absorption window had significantly
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29 431 positive effects towards improving the oral bioavailability. Delayed gastric emptying had also
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32 432 caused extended absorption phase resulting in T_{max} of 7 h. It is also noteworthy that the
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34 433 variability in the bioavailability was reduced at fed state (Table 3), which is crucial for drugs
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36 434 such as CDK inhibitors where the narrow therapeutic window is a limitation [32].

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41 436 To note, there could be interspecies differences between the rats and the humans in the
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44 437 gastrointestinal physiology and luminal contents which might result in different food effects.
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46 438 However, the changes of pH between fasted and fed states are similar between the two species
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49 439 and the rat intestinal fluid has slightly higher concentration of bile salt and phospholipid
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51 440 compared to the FeSSIF [17, 42, 43]. Therefore, similar pattern of food effect could be expected
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53 441 in humans although the extent might vary.

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444 **5. Conclusion**

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2 445 In conclusion, this study demonstrates an *in vitro-in vivo-in silico* approach in improving the
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5 446 oral bioavailability of DF030263, a promising candidate for treatment of CLL. The two-site
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7 447 absorption windows hypothesis was suggested and supported by *in vitro* and *in silico* studies
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10 448 following observation of a double-peak phenomenon *in vivo*. Exploitation of the two-site
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12 449 absorption was attempted in order to improve the bioavailability. Colonic administration
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14 450 confirmed that the large intestine is a second absorption window but indicated that controlled
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17 451 release to the colon would not enhance the drug exposure. Instead, oral administration at fed
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19 452 state took advantage of the food-effect in terms of improved solubilization, reduced
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22 453 precipitation and delayed gastrointestinal transit time, thereby increasing the bioavailability.
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28
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31
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474 **References**

- 475 1. Lammers, T., W.E. Hennink, and G. Storm, *Tumour-targeted nanomedicines: principles and practice*. Br. J. Cancer, 2008. **99**(3): p. 392-7.
- 477 2. Thanki, K., et al., *Oral delivery of anticancer drugs: challenges and opportunities*. J. Control. Release, 2013. **170**(1): p. 15-40.
- 479 3. Li, J., et al., *A review on various targeted anticancer therapies*. Target Oncol, 2012. **7**(1): p. 69-85.
- 481 4. Ruddy, K., E. Mayer, and A. Partridge, *Patient adherence and persistence with oral anticancer treatment*. CA. Cancer J. Clin., 2009. **59**(1): p. 56-66.
- 483 5. Banna, G.L., et al., *Anticancer oral therapy: emerging related issues*. Cancer Treat. Rev., 2010. **36**(8): p. 595-605.
- 485 6. O'Neill, V.J. and C.J. Twelves, *Oral cancer treatment: developments in chemotherapy and beyond*. Br. J. Cancer, 2002. **87**(9): p. 933-7.
- 487 7. Lapenna, S. and A. Giordano, *Cell cycle kinases as therapeutic targets for cancer*. Nat. Rev. Drug Discov., 2009. **8**(7): p. 547-66.
- 489 8. Shao, H., et al., *Substituted 4-(thiazol-5-yl)-2-(phenylamino)pyrimidines are highly active CDK9 inhibitors: synthesis, X-ray crystal structures, structure-activity relationship, and anticancer activities*. J Med Chem, 2013. **56**(3): p. 640-59.
- 492 9. Shao, H., et al., *Synthesis, structure-activity relationship and biological evaluation of 2,4,5-trisubstituted pyrimidine CDK inhibitors as potential anti-tumour agents*. Eur J Med Chem, 2013. **70**: p. 447-55.
- 495 10. Wang, S. and P.M. Fischer, *Cyclin-dependent kinase 9: a key transcriptional regulator and potential drug target in oncology, virology and cardiology*. Trends Pharmacol. Sci., 2008. **29**(6): p. 302-13.
- 498 11. Shao, H., et al., *Structure-based design of highly selective 2,4,5-trisubstituted pyrimidine CDK9 inhibitors as anti-cancer agents*. Eur J Med Chem, 2021. **214**: p. 113244.
- 501 12. Dressman, J.B., et al., *Estimating drug solubility in the gastrointestinal tract*. Adv Drug Deliv Rev, 2007. **59**(7): p. 591-602.
- 503 13. Vertzoni, M., et al., *Simulation of fasting gastric conditions and its importance for the in vivo dissolution of lipophilic compounds*. Eur J Pharm Biopharm, 2005. **60**(3): p. 413-7.

- 506 14. Merchant, H.A., et al., *Gastrointestinal characterisation and drug solubility*
1 507 *determination in animals*. J Pharm Pharmacol, 2015. **67**(5): p. 630-9.
- 3 508 15. Kagan, L. and A. Hoffman, *Selection of drug candidates for gastroretentive dosage*
4 509 *forms: pharmacokinetics following continuous intragastric mode of administration in*
5 510 *a rat model*. Eur J Pharm Biopharm, 2008. **69**(1): p. 238-46.
- 7 511 16. Smith, H.W., *Observations on the Flora of the Alimentary Tract of Animals and*
8 512 *Factors Affecting Its Composition*. J Pathol Bacteriol, 1965. **89**: p. 95-122.
- 10 513 17. Ward, F.W. and M.E. Coates, *Gastrointestinal pH measurement in rats: influence of*
11 514 *the microbial flora, diet and fasting*. Lab Anim, 1987. **21**(3): p. 216-22.
- 13 515 18. Evans, D.F., et al., *Measurement of gastrointestinal pH profiles in normal ambulant*
14 516 *human subjects*. Gut, 1988. **29**(8): p. 1035-41.
- 16 517 19. Agoram, B., W.S. Woltosz, and M.B. Bolger, *Predicting the impact of physiological*
17 518 *and biochemical processes on oral drug bioavailability*. Advanced Drug Delivery
18 519 Reviews, 2001. **50**: p. S41-S67.
- 20 520 20. Clements, J.A., et al., *Kinetics of acetaminophen absorption and gastric emptying in*
21 521 *man*. Clin Pharmacol Ther, 1978. **24**(4): p. 420-31.
- 23 522 21. Wang, Y., et al., *A double-peak phenomenon in the pharmacokinetics of alprazolam*
24 523 *after oral administration*. Drug Metab Dispos, 1999. **27**(8): p. 855-9.
- 26 524 22. Takamatsu, N., et al., *Variability in cimetidine absorption and plasma double peaks*
27 525 *following oral administration in the fasted state in humans: correlation with antral*
28 526 *gastric motility*. Eur J Pharm Biopharm, 2002. **53**(1): p. 37-47.
- 30 527 23. Ogiso, T., et al., *Pharmacokinetics of epinastine and a possible mechanism for double*
31 528 *peaks in oral plasma concentration profiles*. Biol Pharm Bull, 2001. **24**(7): p. 790-4.
- 33 529 24. Hammarlund, M.M., L.K. Paalzow, and B. Odland, *Pharmacokinetics of furosemide*
34 530 *in man after intravenous and oral administration. Application of moment analysis*.
35 531 Eur J Clin Pharmacol, 1984. **26**(2): p. 197-207.
- 37 532 25. Lennernas, H. and C.G. Regardh, *Regional gastrointestinal absorption of the beta-*
38 533 *blocker pafenolol in the rat and intestinal transit rate determined by movement of*
39 534 *¹⁴C-polyethylene glycol (PEG) 4000*. Pharm Res, 1993. **10**(1): p. 130-5.
- 41 535 26. Yin, O.Q., et al., *A modified two-portion absorption model to describe double-peak*
42 536 *absorption profiles of ranitidine*. Clin Pharmacokinet, 2003. **42**(2): p. 179-92.
- 44 537 27. Plusquellec, Y., et al., *A double-peak phenomenon in the pharmacokinetics of*
45 538 *veralipride after oral administration: a double-site model for drug absorption*. J
46 539 Pharmacokinet Biopharm, 1987. **15**(3): p. 225-39.
- 48
49
50
51
52
53
54
55
56
57
58
59
60
61
62
63
64
65

- 540 28. Wagner, J.G., *Unusual pharmacokinetics*, in *Pharmacokinetics: A Modern View*, L.Z.
1 541 Benet, G. Levy, and B.L. Ferraiolo, Editors. 1984, Plenum Press: New York. p. 173-
2 542 189.
- 3 543 29. Godfrey, K.R., et al., *Modelling the Double Peak Phenomenon in pharmacokinetics*.
4 544 Comput Methods Programs Biomed, 2011. **104**(2): p. 62-9.
- 5 545 30. Williams, M.F., et al., *Influence of gastrointestinal site of drug delivery on the*
6 546 *absorption characteristics of ranitidine*. Pharm Res, 1992. **9**(9): p. 1190-4.
- 7 547 31. Charman, W.N., et al., *Absorption of danazol after administration to different sites of*
8 548 *the gastrointestinal tract and the relationship to single- and double-peak phenomena*
9 549 *in the plasma profiles*. J Clin Pharmacol, 1993. **33**(12): p. 1207-13.
- 10 550 32. Guha, M., *Cyclin-dependent kinase inhibitors move into Phase III*. Nat Rev Drug
11 551 Discov, 2012. **11**(12): p. 892-4.
- 12 552 33. Roush, J.A., *Evaluation of gastrointestinal motility directly from human*
13 553 *pharmacokinetic data*. Int J Pharm, 2011. **419**(1-2): p. 43-51.
- 14 554 34. Kakhi, M. and J. Chittenden, *Modeling of pharmacokinetic systems using stochastic*
15 555 *deconvolution*. J Pharm Sci, 2013. **102**(12): p. 4433-43.
- 16 556 35. Heikkinen, A.T., et al., *Application of PBPK modeling to predict human intestinal*
17 557 *metabolism of CYP3A substrates - an evaluation and case study using GastroPlus*.
18 558 Eur J Pharm Sci, 2012. **47**(2): p. 375-86.
- 19 559 36. Mathias, N.R. and J. Crison, *The use of modeling tools to drive efficient oral product*
20 560 *design*. AAPS J, 2012. **14**(3): p. 591-600.
- 21 561 37. Parrott, N., et al., *Application of full physiological models for pharmaceutical drug*
22 562 *candidate selection and extrapolation of pharmacokinetics to man*. Basic Clin
23 563 Pharmacol Toxicol, 2005. **96**(3): p. 193-9.
- 24 564 38. De Buck, S.S., et al., *Prediction of human pharmacokinetics using physiologically*
25 565 *based modeling: a retrospective analysis of 26 clinically tested drugs*. Drug Metab
26 566 Dispos, 2007. **35**(10): p. 1766-80.
- 27 567 39. Suttle, A.B. and K.L. Brouwer, *Regional gastrointestinal absorption of ranitidine in*
28 568 *the rat*. Pharm Res, 1995. **12**(9): p. 1311-5.
- 29 569 40. Davis, S.S., *Formulation strategies for absorption windows*. Drug Discov Today,
30 570 2005. **10**(4): p. 249-57.
- 31 571 41. Kostewicz, E.S., et al., *Predicting the precipitation of poorly soluble weak bases upon*
32 572 *entry in the small intestine*. J Pharm Pharmacol, 2004. **56**(1): p. 43-51.
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573 42. Berghausen, J., et al., *Simulated rat intestinal fluid improves oral exposure prediction*
1 574 *for poorly soluble compounds over a wide dose range.* *Admet & Dmpk*, 2016. **4**(1): p.
2 35.
3 575
4
5 576 43. McConnell, E.L., A.W. Basit, and S. Murdan, *Measurements of rat and mouse*
6 *gastrointestinal pH, fluid and lymphoid tissue, and implications for in-vivo*
7 577 *experiments.* *J Pharm Pharmacol*, 2008. **60**(1): p. 63-70.
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