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Citation for final published version:

Genc, Sila, Ball, Gareth, Chamberland, Maxime , Raven, Erika P., Tax, Chantal M. W. , Ward, Isobel, Yang, Joseph Y. M., Palombo, Marco and Jones, Derek K. 2025. MRI signatures of cortical microstructure in human development align with oligodendrocyte cell-type expression. Nature Communications Item availability restricted.

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MRI signatures of cortical microstructure in human development align with oligodendrocyte cell-type expression

Sila Genc^{1,2,3}, Gareth Ball^{2,4}, Maxime Chamberland^{1,5}, Erika P Raven^{1,6}, Chantal MW Tax^{1,7}, Isobel Ward^{1,8}, Joseph YM Yang^{2,3,4}, Marco Palombo¹, Derek K Jones¹

1. Cardiff University Brain Research Imaging Centre (CUBRIC), Cardiff University, Cardiff, United Kingdom

2. Developmental Imaging, Clinical Sciences, Murdoch Children's Research Institute, Parkville, Victoria, Australia

3. Neuroscience Advanced Clinical Imaging Service (NACIS), Department of Neurosurgery, The Royal Children's Hospital, Parkville, Victoria, Australia

4. Department of Paediatrics, University of Melbourne, Parkville, Victoria, Australia

5. Eindhoven University of Technology, Department of Mathematics and Computer Science, Eindhoven, The Netherlands

6. Center for Biomedical Imaging, Department of Radiology, New York University Grossman School of Medicine, New York, USA

7. Image Sciences Institute, University Medical Center Utrecht, Utrecht, The Netherlands

8. Data and Analysis for Social Care and Health, Office for National Statistics, Newport, United Kingdom

Abstract

Neuroanatomical changes to the cortex during adolescence have been well documented using MRI, revealing ongoing cortical thinning and volume loss. Recent advances in MRI hardware and new biophysical models of tissue informed by diffusion MRI data hold promise for identifying the cellular changes driving these morphological observations. Using ultra-strong gradient MRI, this study quantified cortical neurite and soma microstructure in typically developing youth. Cortical neurite signal fraction, attributed to neuronal and glial processes, increased with age (mean $R^2_{\text{neurite}}=.53$, $p<3.3e-11$, 11.91% increase over age), while apparent soma radius decreased (mean $R^2_{\text{Rsoma}}=.48$, $p<4.4e-10$, 1% decrease over age) across domain-specific networks. Analyses of two independent post-mortem datasets revealed that genes increasing in expression through adolescence were significantly enriched in cortical oligodendrocytes and Layer 5-6 neurons. Here, we show spatial and temporal alignment of oligodendrocyte cell-type gene expression with neurite and soma microstructural changes, suggesting that ongoing cortical myelination processes drive adolescent cortical development.

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48 1. Context

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50 Over the last two decades, magnetic resonance imaging (MRI) has provided
51 invaluable insights into the developing brain, revealing ongoing cortical thinning and
52 cortical volume loss throughout adolescence (Mills et al., 2016; Tamnes et al.,
53 2017). However, the underlying cellular processes driving these changes are less
54 understood. Cortical cytoarchitecture can be broadly categorised into neurites (e.g.,
55 axons, dendrites, and glial processes) and soma (e.g., neuronal, and glial cell
56 bodies). Traditionally, synaptic pruning has been considered the primary driver of
57 developmental changes in cortical morphology (Huttenlocher, 1979). Recent evidence,
58 however, suggests that myelin encroachment into the grey/white matter boundary may
59 also contribute to changes in MR contrast typically used for volumetrics, such as T_1
60 (Natu et al., 2019). Developmental patterns of cortical myelination have been
61 elucidated using magnetization transfer (MT) imaging (Paquola et al., 2019), and
62 indirectly using T1w/T2w ratio (Grydeland et al., 2019). Despite these advances, how
63 microstructural changes - specifically neurite and soma properties - contribute to
64 these distinct morphological changes remains unclear.

65

66 Diffusion-weighted MRI (dMRI) is the main non-invasive MRI technique capable of
67 probing the tissue microstructure, orders of magnitude smaller than the typical
68 millimetre image resolution of structural MRI (Le Bihan et al., 2001). This
69 microstructural imaging method is highly sensitive to the magnitude and direction of
70 water diffusing within brain tissue. By employing biophysical models, it is possible to
71 infer microscopic properties of different tissues, such as neurite signal fraction in the
72 brain's white matter (Alexander et al., 2019; Zhang et al., 2012). In comparison with
73 white matter, grey matter cytoarchitecture, broadly categorized into neurites (e.g.,
74 elongated structures such as axons, dendrites and glial processes) and soma (e.g.,
75 spherical structures such as neuronal and glial cell-bodies) is more locally complex,
76 requiring extensions of the standard models of microstructure developed for studying
77 the white matter. Recent hardware (Fan et al., 2022; Jones et al., 2018) and
78 biophysical modelling (Jelescu et al., 2022; Palombo et al., 2020; Tax et al., 2020)
79 developments have enabled diffusion-weighted microstructural quantification of soma
80 and neurite components in the cortex in vivo. The Soma and Neurite Density
81 Imaging (SANDI; Palombo et al. (2020)), is robust, reliable (Genc et al., 2021),
82 clinically feasible for sufficiently short diffusion times (Schiavi et al., 2023) and has
83 been validated in ex vivo data (lanuş et al., 2022).

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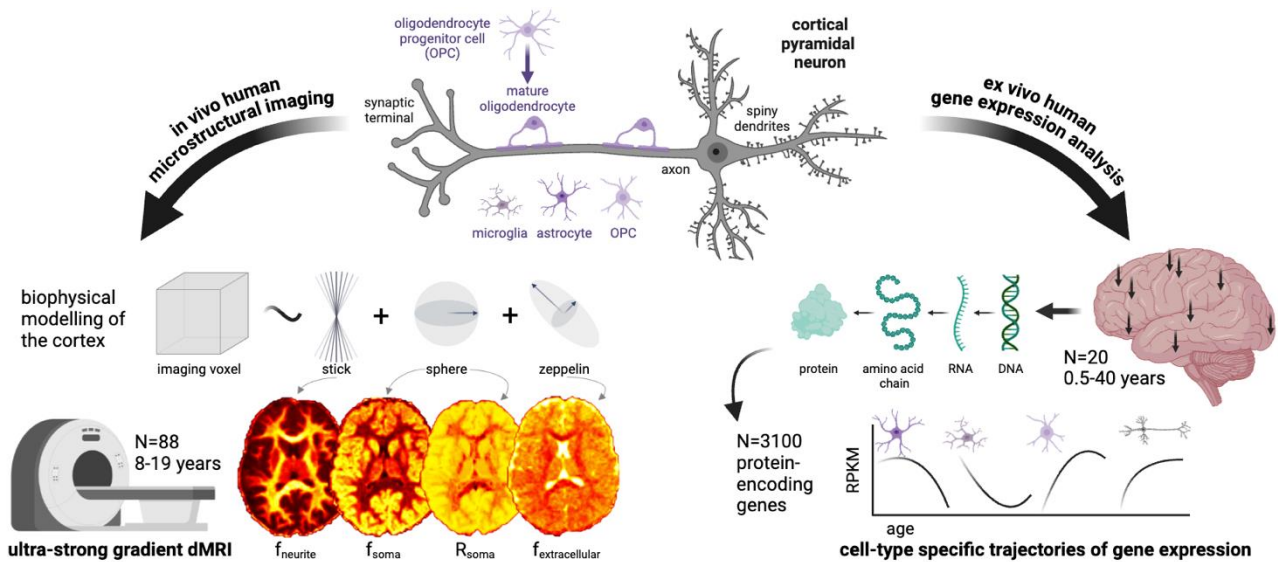
85 SANDI is a biophysical tissue model that estimates the diffusion-weighted signal
86 contribution from three distinct compartments: intra-neurite, intra-soma, and extracellular
87 space. For each imaging voxel, a signal fraction will be estimated for each of the
88 three compartments, such that they sum to 1. In the cortical grey matter, there is
89 a higher proportion of soma (neuronal and glial cell bodies) to neurites, leading to
90 a higher soma signal fraction. These signal fractions vary around tissue boundaries,
91 with higher extracellular signal fraction around the cortical surface due to partial
92 voluming with CSF. Overall, these compartment-specific signal fractions are relative,
93 and comparing these trends over age are potentially meaningful to deduce the
94 compartments that are contributing most to age-related changes in cortical
95 development.

96
97 Here, we examine cortical microstructural development in a sample of children and
98 adolescents using ultra-strong gradient dMRI to identify specific changes in neurite
99 and soma properties with age. To identify potential cellular substrates, we analyse
100 developmental patterns of neurite and soma microstructure alongside contemporaneous
101 trajectories of cortical cell-type specific gene expression measured in the developing
102 cortex using data from two independent, post-mortem databases. We reveal key
103 developmental patterns in cortical neurite and soma architecture, highlighting the
104 contribution of active and ongoing cortical myelination processes to the macroscale
105 changes observed in the cortex during adolescence.

106
107 **2. Results**

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109 We apply a framework for cortical microstructure and cell-type specific gene
110 expression analysis (Fig 1) to evaluate the cellular properties underpinning human
111 cortical microstructural development.

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116 **Figure 1: Framework for cortical microstructure and gene expression analysis.** This study employs a
 117 biophysical model of cortical neurite and soma microstructure using ultra-strong gradient dMRI
 118 (Jones et al., 2018) data collected from 88 children and adolescents aged 8-19 years.
 119 Representative maps of neurite signal fraction (f_{neurite}), soma signal fraction (f_{soma}), apparent soma
 120 radius (R_{soma} , μm) and extracellular signal fraction ($f_{\text{extracellular}}$) are shown for one 8-year-old female
 121 participant. We also analyse two human gene expression datasets (Colantuoni et al., 2011; Li et
 122 al., 2018) to estimate cell-type specific and spatial (where arrows on brain render indicate a
 123 subset of regions sampled) gene expression profiles and examine their concordance with
 124 developmental patterns of cortical microstructure.

125

126 2.1. Cortical microstructure and morphology in domain-specific networks

127

128 First, we studied the repeatability of cortical microstructural estimates from the SANDI
 129 model in a sample of 6 healthy adults scanned over 5 sessions. Intra-class
 130 coefficients (ICCs) for neurite signal fraction (f_{neurite}), soma signal fraction (f_{soma}) and
 131 extracellular signal fraction ($f_{\text{extracellular}}$) were very high (Fig 2c) across seven domain-
 132 specific networks (mean ICC=.97, all $p < .001$). Apparent soma radius (R_{soma} , in μm)
 133 showed lower repeatability on average (mean ICC=.92) with lower mean repeatability
 134 driven by the limbic network.

135

136 We then studied age-related patterns of cortical microstructure and morphology in a
 137 sample of 88 typically developing children and adolescents aged 8-19 years (Table
 138 S2). Cortical f_{neurite} and intracellular volume fraction (v_{ic} ; derived from the NODDI
 139 model, Zhang et al. (2012)) increased with age across all cortical networks (mean
 140 $R^2_{\text{neurite}} = .53$, all networks $p < 3.3e-11$; mean $R^2_{\text{vic}} = .46$, all networks $p < 1.6e-9$) (Fig 2d,
 141 Fig S1). Orientation dispersion index (ODI; derived from the NODDI model, Zhang et
 142 al. (2012)) also increased with age across all studied networks (mean $R^2_{\text{odi}} = .42$, all
 143 networks $p < 1.9e-5$). In contrast, we observed decreasing R_{soma} with age across all

144 networks (mean $R^2_{R_{\text{soma}}}=.48$, all networks $p<4.4e-10$) and f_{soma} decreased with age in
145 the dorsal attention ($R^2_{f_{\text{soma}}}=.12$), limbic ($R^2_{f_{\text{soma}}}=.09$) and somatomotor ($R^2_{f_{\text{soma}}}=.23$),
146 networks (all $p<.002$). $f_{\text{extracellular}}$ decreased in the default mode ($R^2_{f_e}=.12$), limbic
147 ($R^2_{f_e}=.21$) and visual ($R^2_{f_e}=.09$) networks (all $p<.004$). DTI metrics revealed decreasing
148 FA with age across all networks apart from the limbic network (mean $R^2 = .27$,
149 $p<2.1e-5$), decreasing MD in the limbic network, $\beta= -.42$, $[-.62, -.22]$, $p=8.8e-5$, and
150 increasing MD in the somatomotor network, $\beta= .34$, $[.13, .55]$, $p=.002$.

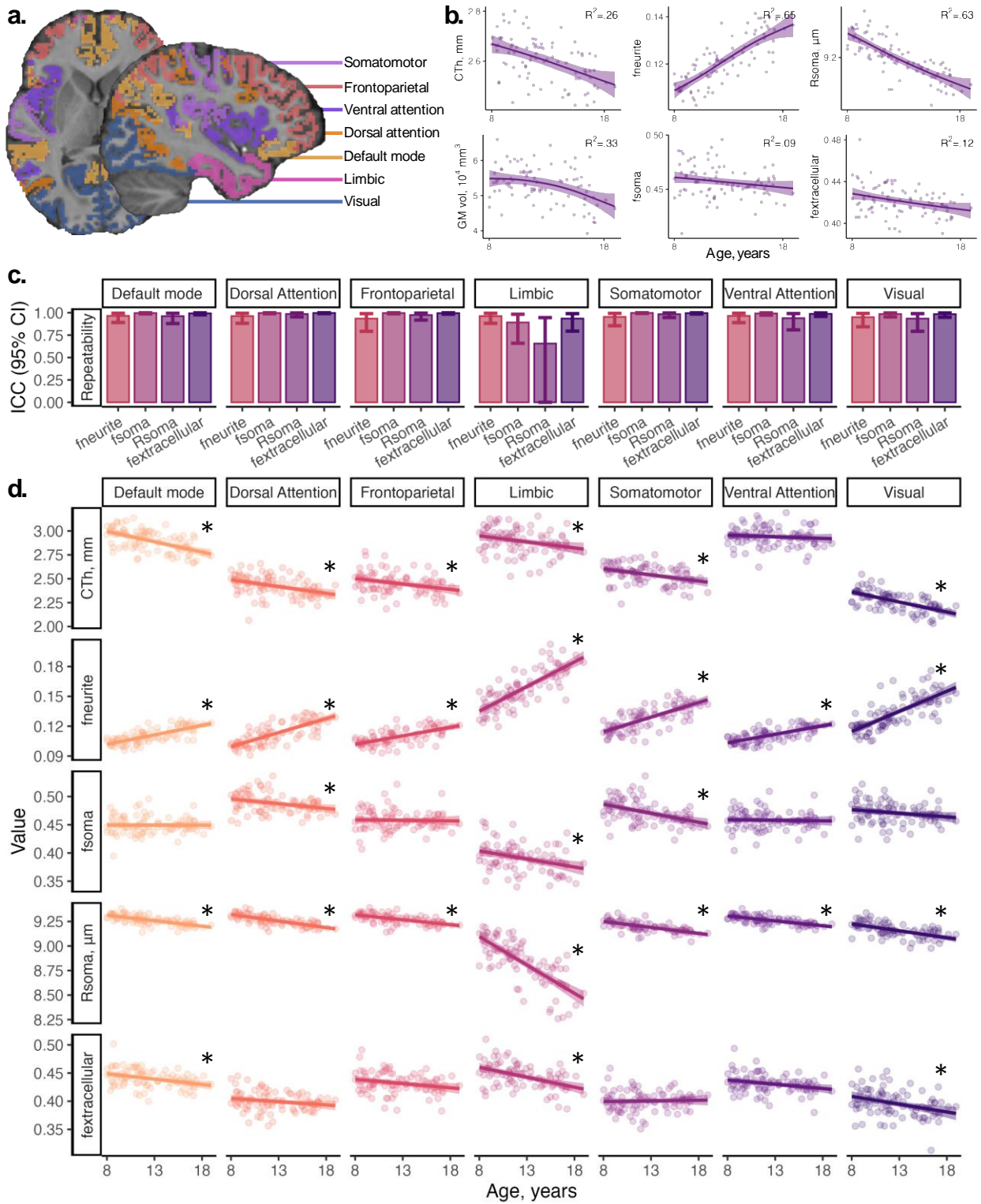
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152 Consistent with established developmental patterns, cortical thickness and grey matter
153 volume decreased with age (Fig 2b). The strength of these associations varied
154 across brain networks (see Fig S1 and Table S2). Specifically, cortical thickness
155 exhibited age-related decline in the default mode, $\beta= -.59$ $[-.77, -.41]$, dorsal
156 attention, $\beta= -.40$ $[-.61, -.19]$, somatomotor, $\beta= -.40$ $[-.60, -.19]$, and visual, $\beta= -.61$
157 $[-.78, -.43]$, networks (all $p<.001$). Similarly, grey matter volume decreased with age
158 in the default mode, $\beta= -.37$ $[-.55, -.20]$, dorsal attention, $\beta= -.34$ $[-.54, -.15]$, and
159 visual $\beta= -.29$ $[-.47, -.11]$, networks (all $p<.002$). Cortical surface area did not show
160 significant age-related differences. The magnitude and direction of age effects across
161 all microstructural and morphological measures are shown in Figure S1.

162

163 Sex differences in brain structure have been well reported, with pubertal onset
164 playing a critical role in initiating developmental changes to morphology (Vijayakumar
165 et al., 2018) and microstructure (Tamnes et al., 2018). We found that grey matter
166 volume and surface area were higher in males than females ($p<.005$) across all
167 brain networks (Figure S2), following known patterns of larger brain volume in
168 males. We observed sex differences in only two microstructural measures, R_{soma} and
169 fractional anisotropy (FA; derived from the diffusion tensor at $b=1200$ s/mm²), in the
170 visual network (Fig S2, S3). Females had higher R_{soma} , $\beta= -.57$ $[-.91, -.24]$, $p=.001$,
171 and lower FA, $\beta= .55$, $[.18, .92]$, $p=.004$, compared to males. We observed a
172 pubertal stage by sex interaction on f_{soma} , where males had lower soma signal
173 fraction in early puberty, $\beta= .73$ $[.28, 1.18]$, $p=.002$, which stabilised in late puberty.
174 Males had lower $f_{\text{extracellular}}$ throughout puberty $\beta= -.74$ $[-1.18, -.31]$, $p=.001$. To further
175 demonstrate developmental differences in the visual network we built an age
176 prediction model (see supplementary section 8.3.2 and Figure S10) which showed
177 that R_{soma} provided the most accurate age-prediction (cross-validated $R^2=.58$). Feature
178 importance revealed top-ranking regions represent cortical endpoints of developmentally
179 sensitive tracts, identified through tractography, such as the posterior corpus callosum,
180 cingulum, and inferior longitudinal fasciculus (Fig S10d).

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Figure 2: Developmental patterns of MRI-derived cortical morphology and microstructure: (a) regions in atlas used to derive domain-specific networks (Yeo et al., 2011) overlaid on a representative participant; (b) developmental patterns of cortical morphology and microstructure averaged across the cortical ribbon; (c) demonstration of high repeatability of SANDI measures in six adults scanned over 5 time-points within two weeks; (d) network-wide patterns of microstructure and morphology, indicating age-related increases in neurite fraction and reductions in cortical thickness, apparent soma radius, soma fraction and extracellular fraction. Significant age relationships ($p < .005$)

190 are annotated (*). Abbreviations: CTh: cortical thickness, in mm; $f_{\text{extracellular}}$: extracellular signal
191 fraction; f_{neurite} : neurite signal fraction; f_{soma} : soma signal fraction; GM: grey matter; ICC: intra-class
192 coefficient; R_{soma} : apparent soma radius, in μm .

193 **2.2. Contemporaneous gene expression trajectories**

194

195 Using $n=214$ post-mortem tissue samples from the dorsolateral prefrontal cortex
196 (DLFPC; BrainCloud; Colantuoni et al. (2011)), we identified $n=2057$ genes with
197 differential expression over the lifespan (0.5 - 72 years; $p_{\text{FDR}} < 0.05$). We validated this
198 selection in an independent RNA-seq dataset (PsychENCODE; Li et al. (2018);
199 $n=20$), identifying $n=467$ (22.7%) genes with significant age-associations in both
200 datasets (age-genes; Supp Info).

201

202 We identified sets of differentially expressed genes across 7 cortical cell-types (see
203 Methods). Mean trajectories of gene expression across ages 0 and 30 years,
204 averaged within each cell-type, are shown as standardized curves in Figure 3 for
205 PsychENCODE (Fig 3a) and BrainCloud (Fig 3b) datasets. Developmental profiles
206 from the DLPFC were visualised, to allow for clearer comparisons of cell-type
207 specific trends over age between cohorts. Non-normalized gene expression curves for
208 PsychENCODE are presented in Figure S4 to aid in interpreting relative differences
209 in gene expression magnitudes. Among genes expressed in excitatory neuronal
210 populations and oligodendrocytes, mean expression levels increased with age. In
211 contrast, genes expressed in inhibitory neurons showed no age-related variation.
212 Genes expressed in endothelial cells, astrocytes, microglia and OPCs, exhibited a
213 decrease in mean gene expression with age. Overall, microglial gene expression
214 (mean $\log_2\text{RPKM} = 1.96$) was lower compared to astrocytes (mean $\log_2\text{RPKM} = 3.70$),
215 oligodendrocytes (mean $\log_2\text{RPKM} = 3.11$), OPCs (mean $\log_2\text{RPKM} = 3.01$), excitatory
216 neurons (mean $\log_2\text{RPKM} = 4.15$) and inhibitory neurons (mean $\log_2\text{RPKM} = 2.94$). To
217 validate our bulk-tissue findings in an independent dataset, we took advantage of a
218 recent single-cell RNA atlas of pre- and postnatal brain development (Velmeshev et
219 al., 2023). Using these data, we identified a set of cell-specific genes with an onset
220 of expression in childhood (>4 years) followed by a rapid increase through
221 adolescence and into adulthood ($n=534$ genes). Most of these genes were expressed
222 by oligodendrocytes ($n=349$; Figure S12), confirming our findings from bulk-tissue
223 data.

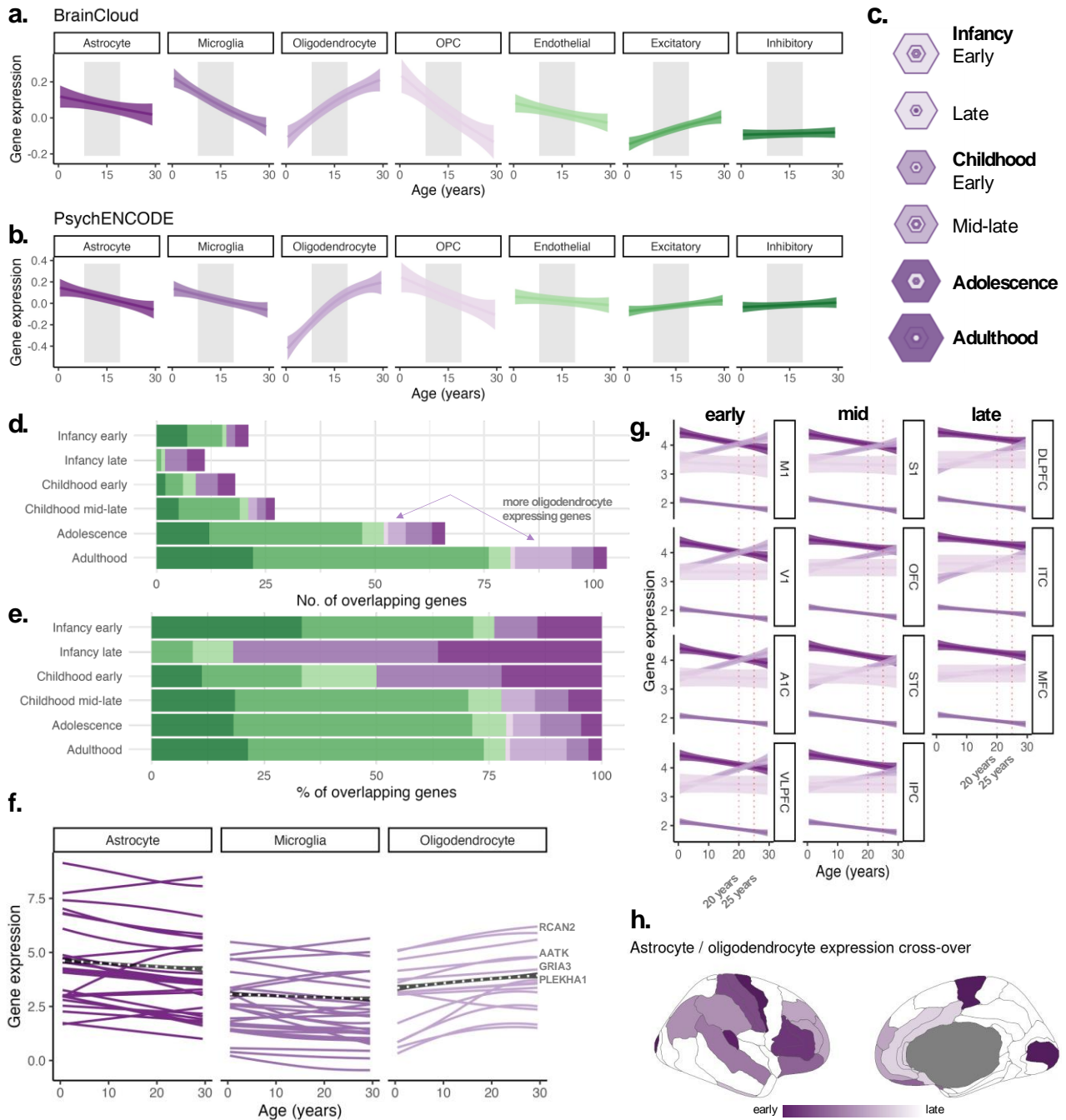
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225 We confirmed the enrichment of cell-types identified in the age-related genes
226 identified using bulk-tissue data using an independent cell-type specific expression
227 analysis (CSEA). Significant enrichment of age-genes ($n=467$) was observed in
228 cortical oligodendrocytes, oligodendrocyte progenitors, and Layer 5-6 neurons (Fig S5).

229 These genes were prominently expressed across developmental stages in childhood
230 adolescence, and young adulthood (Fig S6, Fig 3c). The number (Fig 3d) and
231 proportion (Fig 3e) of age-related genes expressed by oligodendrocytes increased
232 significantly in adolescence and young adulthood (Fig 3d,e). These included genes
233 associated with CNS (re)myelination, RCAN2 (Huang et al., 2011), GRIA3
234 (Kougioumtzidou et al., 2017), and the differentiation of OPCs and oligodendrocytes,
235 PLEHA1/TAPP1 (Chen et al., 2015); AATK/AATYK (Jiang et al., 2018).

236

237 For each cell-type, we quantified the spatiotemporal patterns of gene expression
238 using PsychENCODE data by identifying the peak growth of expression in cell-
239 specific genes. Oligodendrocyte gene expression peaked earliest in primary motor
240 (M1), primary visual (V1) cortices, and latest in the medial frontal (MFC) cortex (Fig
241 S8). A notable pattern emerged in which the peak expression of oligodendrocyte
242 genes coincided with a shift in oligodendrocyte-to-astrocyte specific expression ratio.
243 This shift, indicating a relative increase in oligodendrocyte over astrocyte cell-type
244 gene expression, occurred around 20 years of age in M1 and V1, and after age
245 25 in DLPFC, ITC and MFC (Fig 3g,h). This sequence aligns with the known
246 earlier myelination timing in sensorimotor cortices followed by prolonged myelination
247 in the pre-frontal cortex into the third decade of life (Grydeland et al., 2019;
248 Paquola et al., 2019; Sydnor et al., 2021).



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251 **Figure 3: Developmental trajectories of cell-type specific gene expression.** Data shown for samples
 252 aged 0-30 years from: (a) BrainCloud (Z-score), and (b) PsychENCODE (expressed in log₂-reads-
 253 per-kilobase of transcript per million (log₂RPKM)) datasets, demeaned to account for overall higher
 254 expression in some cell-types. Age effects were modelled in all postnatal samples to maximise
 255 sample size. Grey shaded areas highlight the age range of the microstructural imaging cohort (8-
 256 19 years) for visual comparison of developmental profiles. (c) SEA results (Xu et al., 2014)
 257 showing significant enrichment of age-related genes through adolescence and adulthood, where
 258 hexagon size scales with enrichment (overlap) of age-related genes in genes expressed by each
 259 cell type, and darker rings indicate significant associations at $p_{FDR} < .001$ with inner rings indicating

260 high cell specificity. Age-related genes overlapping postnatal developmental stages are shown as
261 (d) total number of genes, and (e) proportion of genes, indicating an increase in neuronal, glial
262 and oligodendrocyte-specific genes. (f) Trajectories of glial genes overlapping the SEA and our
263 age-genes. (g) Regional shifts in the glial cell-type expression ratio ($\log_2\text{RPKM}$) across
264 development, with the astrocyte-to-oligodendrocyte expression ratio crossing earliest at age 20
265 years in primary motor and visual cortices. (h) Timing of this cross-over, with darker values
266 indicating regions with an earlier crossing point. Note that white coloured regions are not
267 represented in the data set.

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269 **2.3. Concordant profiles of microstructure and gene expression indicate developmental** 270 **cortical myelination**

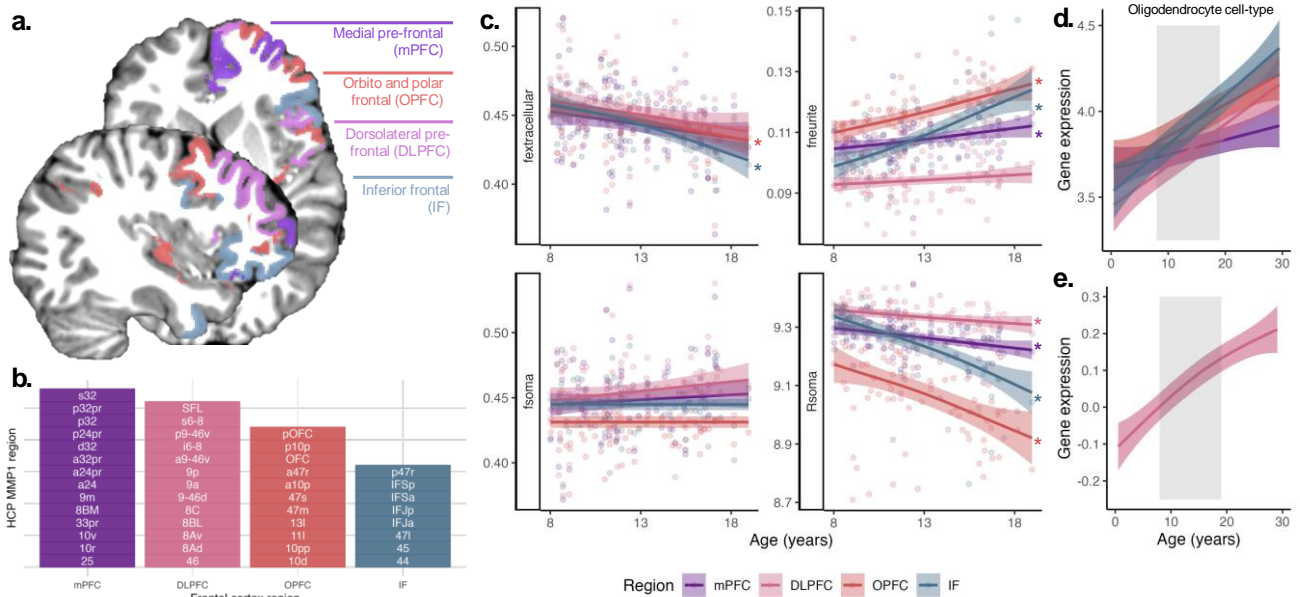
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272 To elucidate the cell-specific basis of our imaging findings, we examined neurite and
273 soma microstructural measures in the same four frontal regions sampled in the
274 PsychENCODE data (MFC, IFC, DLPFC, VLPFC; see Fig 4a,b) using a fine-grained
275 parcellation of the frontal lobe. Microstructural MRI revealed regional increases in
276 f_{neurite} and decreases in R_{soma} (Fig 4c). This pattern corresponded with increased
277 regional oligodendrocyte cell-type gene expression profiles in the same regions over
278 the same age period (Fig 4d,e). The spatial distribution of oligodendrocyte cell-type
279 expression was aligned with regional differences in peak growth of the neurite
280 fraction (Fig S7). Thus, the dMRI-derived neurite signal fraction likely reflects
281 spatiotemporal patterns of cortical myelination, matching the peak expression of
282 oligodendrocyte-genes.

283

284 To further evaluate the concordance between in vivo MRI and ex vivo gene
285 expression patterns, we performed numerical simulations using realistic cell counts to
286 explain age-related patterns of the apparent soma radius. Assuming that the
287 observed age-related slope of gene expression was proportional to the number of
288 cells of each cell-type within an MRI voxel, we modelled cell-type composition
289 changes based on the actual expected distribution of cell body radii within a voxel
290 based on realistic cell counts and sizes. Our results revealed close correspondence
291 between simulated and in vivo modelling results of R_{soma} (Fig S9), showing a 1%
292 age-related decrease in both simulated and dMRI-derived data across 8-19 years.

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Figure 4: Regional variation of microstructure and gene expression in the frontal cortex. (a) Structural MRI-based segmentation of four frontal regions: medial pre-frontal cortex (mPFC); dorsolateral prefrontal cortex (DLPFC); orbito and polar frontal cortex (OPFC), and inferior frontal cortex (IF); (b) sub-regions from the HCP-MMP1 atlas (Glasser et al., 2016), which comprised the regions in (a); (c) age-related patterns of microstructural measures (*: $p < 0.005$); oligodendrocyte cell-type gene expression in (d) PsychENCODE data sampled in the same 4 frontal cortical regions as (a), and (e) BrainCloud data sampled in the DLPFC.

3. Discussion

We combined in vivo ultra-strong gradient dMRI with independent ex vivo gene expression analyses to map tissue microstructural architecture during human development. We now discuss each of the key findings and their implications, before summarising the strengths and limitations of our study.

Neurite Signal Fraction Increases from Childhood to Adolescence

The neurite signal fraction, f_{neurite} , attributed to elongated cortical structures (e.g., axons, processes), increased with age across the whole cortex, but peaked earliest in the visual and somatomotor networks, mirroring previous findings (Lynch et al., 2024). Intracortical myelination continues over adolescence (Bartzokis, 2012; Gibson et al., 2014; Grydeland et al., 2019; Natu et al., 2019; Whitaker et al., 2016), following a stereotyped sensorimotor-to-association (S-A) axis of development (Sydnor et al., 2023). Although dMRI is relatively insensitive to water within the myelin sheath itself, due to its short T_2 (D. K. Jones et al., 2013), the observed increase in f_{neurite} may nevertheless reflect intra-cortical myelination. This is supported by ex vivo macaque data showing developmental increases in glial process length and complexity (Robillard et al., 2016), and an increase in the number of myelinated

323 axons and dendrites (Fukutomi et al., 2018), which limits water exchange and leads
324 to a greater signal contribution from inside the neurite (Jelescu et al., 2022; Olesen
325 et al., 2022).

326

327 **Oligodendrocyte-Specific Gene Expression Increases from Childhood to Adolescence**

328 Supporting our in vivo MRI findings, oligodendrocyte-specific gene expression
329 increased with age (Fig 4a,b), aligning with previous observations in independent
330 data (Paquola et al., 2019). Age-related genes were also enriched in cortical
331 neurons (layers 5 and 6) and OPCs (Fig S6). The concordance between the human
332 bulk-tissue gene expression analysis (Fig S5), human single-cell RNA analysis (Fig
333 S12), and the CSEA analysis based on mouse transcriptomic profiling (Fig S6)
334 indicates conservation of myelination processes via cortical oligodendrocytes.

335 Oligodendrocyte cell turnover in the frontal cortex is dynamic, especially in adulthood,
336 and 10 times higher in the cortex than in the white matter (Yeung et al., 2014).

337 OPCs can generate myelinating oligodendrocytes in adulthood, even in fully
338 myelinated regions (Richardson et al., 2011; Young et al., 2013). Importantly,
339 oligodendrocyte function is not restricted to myelination, rather, they also perform
340 many critical neuronal support functions beyond myelination (Bradl & Lassmann,
341 2010). Together our microstructural MRI and gene-expression findings converge
342 towards increased cortical myelination through adolescence.

343

344 **Apparent Soma Radius Decreases from Childhood to Adolescence**

345 The dMRI-derived apparent soma radius, R_{soma} , decreased cortex-wide from childhood
346 to adolescence. Neuronal soma are much larger than glial soma, measuring $\sim 16\mu\text{m}$
347 in diameter in layers 5-6 of the adult human prefrontal cortex, whereas glial soma
348 range in diameter from 1-11 μm (Rajkowska et al., 1998). Our gene expression
349 analysis suggests specific changes in the cellular composition of the cortex with age:
350 decreasing expression levels for astrocyte, microglia and endothelial cell-types, and
351 (much larger) increasing expression levels for oligodendrocyte cell-types. Glial
352 composition in the neocortex is mostly comprised of oligodendrocytes ($\sim 75\%$),
353 followed by astrocytes ($\sim 20\%$) and a smaller prevalence of microglia ($\sim 5\%$) (Pelvig
354 et al., 2008). Assuming gene expression levels are proportional to cell
355 number/density, our observations suggest a decrease in large-soma cells (e.g.,
356 endothelial), outweighed by a larger increase in small-soma cells (e.g.,
357 oligodendrocytes).

358

359 The estimated R_{soma} is dependent on the higher order moments of the soma radii
360 distribution (i.e. skewedness and tailedness) within an MRI voxel (Olesen et al.,

361 2022). Our own simulations of R_{soma} based on known cell composition in the human
362 brain (Keller et al., 2018) revealed a decrease in apparent soma radii with age
363 matching our in vivo imaging observations (i.e., a 1% decrease). This would in turn
364 lead to a reduction in the measured dMRI signal coming from water molecules fully
365 restricted in soma, aligning with our in vivo observations of decreasing f_{soma} with
366 age in the limbic, somatomotor, and dorsal attention networks. It is plausible that an
367 increase in oligodendrocyte (Peters & Sethares, 2004), not astrocyte or microglial
368 (Robillard et al., 2016), composition could concomitantly result in a smaller average
369 soma radii and lower soma signal fraction in the cortex through adolescence to
370 early adulthood.

371

372 **Sex Differences in Microstructural Properties**

373 Females have larger apparent soma radii than males, and f_{soma} and $f_{\text{extracellular}}$ varies
374 with pubertal stage in the visual network (Fig S10a). Pubertal hormones can
375 stimulate apoptosis (seen in female rat visual cortex; Nunez et al. (2002)), which
376 could explain the lower f_{soma} as puberty progresses in females. Selective neuronal
377 cell death with unchanged glial cell number can also occur during puberty in the
378 medial pre-frontal cortex (Markham et al., 2007; Willing & Juraska, 2015), however
379 we did not observe any sex or pubertal differences in microstructure of the frontal
380 cortex.

381

382 **Extracellular Signal Fraction and Myelination**

383 In dMRI, myelin thickening can decrease the extracellular signal fraction, due to less
384 physical space in the extracellular matrix (Jelescu et al., 2016; Derek K Jones et
385 al., 2013). Age-related decreases in $f_{\text{extracellular}}$ were confined to the visual network and
386 orbito-frontal and inferior frontal cortices. Comprehensive evaluation of the myelin
387 content is warranted to confirm the contributions of intracortical myelination to
388 developmental changes in cortical morphology (Mancini et al., 2020).

389

390 **Spatiotemporal Patterns of Gene Expression**

391 Peak oligodendrocyte cell-type gene expression progressed along the S-A axis, with
392 earliest peaks in M1 and V1, and latest in MFC (Fig S8), mirroring spatial patterns
393 of peak f_{neurite} (Fig S7). This also coincided with a relative age-related decrease in
394 astrocyte cell-type gene expression (Fig 4g) consistent with early-life maturation of
395 astrocytes (Bushong et al., 2004; Cahoy et al., 2008). The S-A developmental axis
396 describes a maturation process from lower-order, primary sensory and motor
397 (unimodal) cortices to higher-order transmodal association cortices, which support
398 complex neurocognitive, and socioemotional functions (Margulies et al., 2016; Sydnor

399 et al., 2021). Prolonged maturation of the pre-frontal cortex has been reported with
400 lower myelin content in fronto-polar cortex compared with visual or somatomotor
401 regions from childhood to adulthood (Miller et al., 2012) indicating later myelination
402 timing. Within the frontal cortex, age-related patterns of microstructural neurite signal
403 fraction and soma radius were prolonged in the MFC and DLPFC (Fig 4c-e). This
404 reflects the value of estimating in vivo neurite signal fraction as these developmental
405 hierarchies have been reproduced across various modalities (Burt et al., 2018; Gao
406 et al., 2020; Satterthwaite et al., 2014; Sydnor et al., 2021; Vaishnavi et al., 2010;
407 Wagstyl et al., 2015), particularly when considering the regions reaching peak
408 maturation earliest and latest. Overall, our combined imaging genetic analyses
409 supports the evidence of an orderly and hierarchical progression of intracortical
410 myelination.

411

412 **Implications for Cortical Thinning**

413 A recent study showed that cortical thinning during development is associated with
414 genes expressed predominantly in astrocytes, microglia, excitatory and inhibitory
415 neurons (Zhou et al., 2023). We observed faster cortical thinning of default-mode
416 and visual networks, consistent with previous studies (Ball, Seidlitz, Beare, et al.,
417 2020; Zhou et al., 2023). Apparent thinning may be a result of the macrostructural
418 shift in the boundary between grey matter and white matter, in this scenario due to
419 myelin encroachment into the cortex (Mournet et al., 2020; Natu et al., 2019). The
420 microstructural composition of the grey matter itself may be better studied by the
421 biophysical models used here.

422

423 ~~Clinical implications~~ **Potential applications**

424 Cortical morphology and myelination abnormalities are linked to various
425 neuropsychiatric disorders (Chen et al., 2024) including schizophrenia (Alexander-Bloch
426 et al., 2014; Wannan et al., 2019) which is characterised by deficiencies in
427 myelination and oligodendrocyte production (Davis et al., 2003; Katsel et al., 2005).
428 One potential future application is to quantify cortical microstructure in such clinical
429 cohorts, especially with adaptations towards clinically feasible acquisition protocols
430 using current state-of-the-art clinical grade 3T systems (Barakovic et al., 2024;
431 Margoni et al., 2023; Schiavi et al., 2023), and with the recent advent of
432 commercial systems with ultra-strong gradients (e.g., Siemens 3T Cima.X; GE 3T
433 MAGNUS). Further strengthening this potential application, schizophrenia patients
434 exhibit downregulation of myelination-related genes (Tkachev et al., 2003) and post-
435 mortem studies have shown reduced oligodendrocyte density in layer 5 of
436 dorsolateral prefrontal cortex compared to healthy controls (Kolomeets & Uranova,

437 2019). Additionally, young children with autism show age-related deficits in cortical
438 T1w/T2w ratios (Chen et al., 2022). Future studies exploring these novel
439 neuroimaging measures may provide valuable insights into cortical based
440 abnormalities.

441

442 **Strengths and limitations**

443 Several methodological advancements have advanced the understanding of underlying
444 compositional changes to cortical microstructure across development in our study. Our
445 repeatability results show that SANDI-derived biophysical signal fractions are highly
446 stable (mean ICC=.97) in a young adult population, and these values are highly
447 concordant with recently reported cortex-wide measurements in a subset of younger
448 adults (Lee et al., 2024). Using in vivo microstructural imaging with ultra-strong
449 gradients ($G_{\max}=300$ mT/m; Jones et al. (2018)), we achieved sensitivity to
450 micrometer-level imaging contrast by maximising SNR and minimising the effect of
451 water exchange (Raven et al., 2023). Although we used a specialised system,
452 recent advancements have enabled these measurements on more accessible, lower-
453 gradient strength MRI systems (e.g. $G_{\max}\geq 80$ mT/m; Schiavi et al. (2023)). Combined
454 with two ex vivo gene expression data sets sampled from the human brain, we
455 provide compelling evidence in favour of a framework for monitoring intra-cortical
456 cellular composition in vivo. Further work should evaluate in vivo imaging acquisition
457 techniques and models that account for water exchange, which can influence
458 biophysical modelling of grey matter compartments.

459

460 Our observation of oligodendrocyte-specific gene expression increasing towards
461 adulthood indicates the value of imaging a broader age range of young adults to
462 fully assess trajectories of in vivo microstructural properties. It is also important to
463 recognise that gene expression patterns do not necessarily correlate with cellular
464 density. Histopathological confirmation is needed to verify cell size and density with
465 biophysical signal fractions, as well as their relevancy to functional gene expression
466 patterns.

467

468 Overall, our study provides novel *in vivo* evidence of distinct developmental
469 differences in neurite and soma architecture, aligning with cell-type specific gene
470 expression patterns observed in *ex vivo* human data. This provides a window into
471 the role of intracortical myelination through adolescence, and how it shapes the
472 developmental patterns of cortical microstructure in vivo.

473

474

475 **4. Methods**

476

477 **4.1. Imaging set**

478 **4.1.1. Participant characteristics**

479

480 We included a sample of 88 typically developing children aged 8-19 years recruited
481 as part of the Cardiff University Brain Research Imaging Centre (CUBRIC) Kids
482 study. The study was approved by the School of Psychology ethics committee at
483 Cardiff University. Participants and their parents/guardians were recruited via public
484 outreach events. Written informed consent was obtained from the primary caregiver
485 of each child participating in the study, and adolescents aged 16-19 years also
486 provided written consent. Children were excluded from the study if they had non-
487 removable metal implants or reported history of a major head injury or epilepsy.

488

489 We administered a survey to parents of all participants, and to children aged 11-19
490 years. The Strengths and Difficulties Questionnaire (SDQ) was used to assess
491 emotional/behavioural difficulties (Goodman, 1997). The Pubertal Development Scale
492 (Petersen et al., 1988) was used to determine pubertal stage (PDSS; Shirtcliff et al.
493 (2009)). Additionally, we measured each child's height and weight to calculate their
494 Body-Mass index (BMI) (kg/m²).

495

496 All children and adolescents underwent in-person training to prepare them for the
497 MRI procedure using a dedicated mock MRI scanner. This protocol was 15-30
498 minutes long, and designed to familiarise them to the scanner environment, to
499 minimize head motion during the scan. All procedures were completed in accordance
500 with the Declaration of Helsinki.

501

502 **Table 1: Characteristics of in vivo imaging cohort.**

Measure	Summary statistics			Age relationship*	
	Mean	SD	Range	R ²	<i>p</i> -value
Age, years [†]	12.56	2.94	8.0 - 19.0		
Pubertal stage (PDSS) [†]	2.89	1.50	1 - 5	.72	<.001
SDQ, total score [†]	6.45	3.90	0 - 19	.01	.60
Body mass index, kg/m ^{2‡}	19.29	3.25	13.7 - 29.2	.25	<.001
FSIQ [^]	108	12.6	86 - 145		

503 † Full sample: N=88 (42 males, 46 females)

504 ‡ Subsample: N=79 (40 males, 39 females)

505 ^ Subsample: N=48 (23 males, 25 females)

506 *Age relationships determined by linear regression.

507

508 4.1.2. Acquisition and processing

509

510 Discovery data: Participants aged 8-19 years (N=88, mean age=12.6 years, 46
511 female) underwent MRI on a 3T Siemens Connectom system with ultra-strong (300
512 mT/m) gradients. Structural T₁-weighted (voxel-size=1x1x1mm³; TE/TR=2/2300 ms) and
513 multi-shell dMRI (TE/TR=59/3000 ms; voxel-size=2x2x2 mm³; $\Delta = 23.3$ ms, $\delta = 7$ ms,
514 b-values = 0 (14 vols), 500, 1200(30 dirs), 2400, 4000, 6000 (60 dirs) s/mm²) data
515 were acquired. Data were acquired in an anterior-posterior (AP) phase-encoding
516 direction, with one additional PA volume. The total acquisition time (across four
517 acquisition blocks) was 16 min 14 s.

518

519 Repeatability data: Six healthy adults aged 24-30 years (3 female) were scanned
520 five times in the span of two weeks (Koller et al., 2021) on the same Siemens
521 Connectom system. Multi-shell dMRI data were collected as above, with an additional
522 20 diffusion directions acquired at b=200 s/ mm².

523

524 Pre-processing of dMRI data followed steps interfacing tools such as FSL (Smith et
525 al., 2004), MRtrix3 (Tournier et al., 2019), and ANTS (Avants et al., 2011) as
526 reported previously (Genc et al., 2020). Briefly, this included denoising, and
527 correction for drift, motion, eddy, and susceptibility-induced distortions, Gibbs ringing
528 artefact, bias field, and gradient non-uniformities. For each subject, the soma and
529 neurite density imaging (SANDI) compartment model was fitted (Palombo et al.,
530 2020) to dMRI data using the SANDI Matlab Toolbox v1.0, publicly available at
531 <https://github.com/palombom/SANDI-Matlab-Toolbox-v1.0>, to compute whole brain maps
532 of neurite, soma and extracellular signal fraction (f_{neurite} , f_{soma} , $f_{\text{extracellular}} = 1 - f_{\text{neurite}} -$
533 f_{soma}); the soma radius (R_{soma} , in μm); and the extracellular and intra-neurite axial
534 diffusivities (D_e and D_{in} , respectively, in $\mu\text{m}^2/\text{ms}$) (Fig 1). To put our results in
535 context with previous studies, the neurite orientation dispersion and density imaging
536 (NODDI) model (Zhang et al., 2012) was fitted to all b-values using the NODDI
537 Matlab toolbox, publicly available at
538 <http://mig.cs.ucl.ac.uk/index.php?n=Tutorial.NODDI matlab> , to estimate the intra-cellular
539 volume fraction (v_{ic}) and orientation dispersion (OD) and diffusion tensor imaging

540 (DTI) metrics were estimated using the $b=1200$ s/mm² shell (Fractional anisotropy
541 (FA); mean diffusivity (MD, in s/mm²)).
542
543 T1-weighted data were processed using FreeSurfer version 6.0
544 (<http://surfer.nmr.mgh.harvard.edu>) and post-processed to obtain network-level (N=7
545 ROIs; Yeo et al. (2011)) and fine-grained cortical parcellations (N=360, HCP-MMP1;
546 (Glasser et al., 2016)). The network-level atlas derivation is detailed in Genc et al.
547 (2024). Briefly, we co-registered the Yeo functional atlas in MNI space to each
548 individual subject's space, to obtain seven functionally relevant cortical canonical
549 networks (visual, somatomotor, dorsal attention, ventral attention, limbic, frontoparietal,
550 default mode network). We chose a functional atlas due to the limitations of
551 structural atlases in capturing fine-grained microstructural variations, enabling better
552 insights into developmental patterns of neural activity and connectivity (Fotiadis et al.,
553 2024). Follow-up analyses using fine-grained HCP-MMP1 parcellations in visual and
554 frontal cortices were performed based on a priori hypotheses of earlier maturation of
555 visual (Natu et al., 2019) and later maturation of frontal (Robillard et al., 2016)
556 cortices, as well as for comparison with gene expression data sampled from multiple
557 regions in the frontal cortex. Morphological measures including cortical thickness
558 (CTh, mm), surface area (SA, mm²), and grey matter volume (GMvol, mm³) were
559 computed at the whole brain, and parcel level. The analysis framework is detailed
560 in Figure 1 and networks studied are depicted in Fig 2a.

561

562 **4.2. Cortical gene expression set**

563

564 Pre-processed, batch-corrected and normalised microarray and bulk RNA-seq data
565 from postmortem human tissue samples were obtained from the BrainCloud
566 (Colantuoni et al., 2011) (n=214; aged 6mo - 78.2y; 144 male; postmortem interval
567 [PMI] = 29.96 [15.28]; RNA integrity [RIN] = 8.14 [0.83]) and PsychENCODE (n=20;
568 6mo-40y; 10 male; PMI = 17.85 [6.75]; RIN = 8.45 [0.79]) projects, respectively (Li
569 et al., 2018). The cortical regions sampled are summarised in Table S1, alongside
570 the approximate concordant Yeo7 parcel. Tissue was collected after obtaining parental
571 or next of kin consent and with approval by the institutional review boards at the
572 Yale University School of Medicine, the National Institutes of Health, and at each
573 institution from which tissue specimens were obtained. Tissue processing is detailed
574 elsewhere (Ball, Seidlitz, O'Muircheartaigh, et al., 2020; Li et al., 2018). Gene
575 expression for PsychENCODE was measured as rates per kilobase of transcript per
576 million mapped (RPKM). Gene expression for Braincloud was preprocessed and

577 normalized following data cleaning and regressing out technical variability (see
578 <https://www.ncbi.nlm.nih.gov/geo/query/acc.cgi?acc=GSE30272>).

579

580 Genes were initially filtered to include only protein-coding genes expressed in cortical
581 cell types (n=3100, Ball, Seidlitz, O’Muircheartaigh, et al. (2020)). Using a database
582 of single-cell RNA-seq studies, we identified genes differentially expressed across
583 major cortical cell types (excitatory and inhibitory neurons, oligodendrocytes,
584 oligodendrocyte precursor cells [OPCs], microglia, astrocytes, and endothelial cells
585 (Ball, Seidlitz, Beare, et al., 2020)).

586

587 **4.3. Statistical analyses**

588 **4.3.1. In vivo imaging**

589

590 For the repeatability analysis, the intra-class correlation coefficient (ICC; two-way
591 random effects, absolute agreement) was computed for assessment of test-re-test
592 repeatability for SANDI and DTI metrics using the ‘psych’ package in R. Lower and
593 upper estimates of each ICC represent the bounds of the 95% confidence interval
594 (CI).

595

596 We used linear regression to test for main effects of age and sex, puberty, and
597 sex by puberty interactions. To identify the most parsimonious model and to avoid
598 over-fitting, we used the Akaike Information Criterion (AIC) (Akaike, 1974), selecting
599 the model with the lowest AIC. Individual general linear models were used to
600 determine age-related differences in cortical thickness and microstructural measures in
601 all seven Yeo networks. Evidence for an association was deemed statistically
602 significant when $p < .005$ (Benjamin et al., 2018). Results from linear models are
603 presented as the normalized coefficient of variation (β) and the corresponding 95%
604 confidence interval [lower bound, upper bound]. We also report the adjusted
605 correlation coefficient of the full model (R^2).

606

607 To identify important regions that contribute to age-related differences in all the
608 studied microstructural measures, we performed age-prediction using a random forest
609 (RF) regressor (5-fold cross-validation) for age prediction with PyCaret
610 (www.pycaret.org). We chose a RF model due their ability to model nonlinear
611 relationships, reduced risk of overfitting, and interpretability of feature importance.
612 Specifically, the depth at which a feature appears as a decision node in a tree
613 provides insight into its relative significance for predicting the target variable (i.e.,
614 age). This allows us to assess the relative contribution of features (i.e., average

615 signal fraction in each HCPMMP1 parcel) to age prediction. For each microstructural
616 measure, we randomly split the data into training and validation sets using an 80-20
617 ratio (total N=88: 70 training; 18 testing). Then, we performed feature scaling to
618 ensure that all input variables (for each HCPMMP1 ROI) were on a similar scale
619 prior to model fitting. The performance of the model was evaluated on the validation
620 dataset. Finally, the features with the largest weight coefficients were extracted to
621 identify specific cortical regions where variance in cortical microstructure was
622 associated with age-related changes.

623

624 **4.3.2. Gene expression profiles**

625

626 To identify genes differentially expressed over age ($p_{\text{FDR}} < .05$), we modelled age-
627 related changes in normalised expression in all available postnatal tissue samples
628 using nonlinear generalised additive models with thin plate splines ($k=5$) (Wood,
629 2003) in R.

630 ***BrainCloud***

631

632 The relationship between normalised gene expression and age was modelled with a
633 nonlinear general additive model (GAM) using a penalised thin-plate spline with a
634 maximum 5 knots:

635

```
636 M1a. gam(expression ~  
637 1 + s(age, k=5, bs='tp')
```

638

639 Note that the available BrainCloud data are already preprocessed to remove variance
640 due to batch and sample effects (see
641 <https://www.ncbi.nlm.nih.gov/geo/query/acc.cgi?acc=GSE30272>).

642

643 ***PsychENCODE***

644

645 We repeated the above models, now with a measure of RNA integrity (RIN) as a
646 confounder, and gene expression defined as $\log_2(\text{RPKM})$. First, we included region
647 as an additional factor to account for spatial variation across the cortex and
648 included donor ID as a random effect to account for repeated samples from the
649 same specimen.

650

```
651 M2a. gam(expression ~  
652 1 + s(age, k=5, bs='tp', by=region, id=1)
```


653 + RIN + sex + region + s(sample, bs='re'), data = data))

654

655 Then, we analysed data only in the DLPFC, for comparison with the BrainCloud
656 geneset.

657

```
658 M2a. gam(expression(DLPFC) ~  
659 1 + s(age, k=5, bs='tp')  
660 + RIN + sex + s(sample, bs='re'), data = data))
```

661

662 We calculated measures of goodness of fit using Akaike Information Criterion (AIC)
663 and Bayesian Information Criterion (BIC) for all gene models.

664

665 Using a set of independent single-cell RNA studies of the human cortex (see Ball,
666 Seidlitz et al. (2020) for details), we identified genes exhibiting differential expression
667 across various cortical cells-types, including excitatory neurons, inhibitory neurons,
668 oligodendrocytes, microglia, astrocytes, and endothelial cells. We then compiled gene
669 lists for each cell-type, comprising genes that are both differentially expressed by
670 that cell-type, and uniquely expressed by that cell-type. Mean trajectories across all
671 cortical regions sampled were computed for each cell-type.

672

673 After identifying age-related genes, we entered our list to an independent cell-type
674 specific expression analysis (CSEA; Xu et al. (2014)) to elucidate: 1) if genes were
675 enriched for specific cell-types, and 2) in which developmental period was gene
676 expression highest.

677

678 4.3.3. Simulations

679

680 We performed numerical simulations using realistic cell counts to explain the
681 observed trends in R_{Soma} derived from in vivo dMRI data. We modelled the
682 variability in cell body sizes within an MRI voxel by generating distributions of radii
683 for microglia, astrocytes, oligodendrocytes, neurons, and endothelial cells. For each
684 cell-type, we assumed the observed age-related slope of gene expression was
685 proportional to the number of cells within an MRI voxel. Based on realistic cell
686 counts outlined in Keller et al. (2018), we set the number of cells in mm^3 as
687 follows: $N_{\text{micro}} = 6,500$; $N_{\text{astro}} = 15,700$; $N_{\text{oligo}} = 12,500$; $N_{\text{neuro}} = 92,000$; $N_{\text{endo}} =$
688 $N_{\text{neuro}} \cdot 0.35$ (Ventura-Antunes et al., 2022). For each cell type, we generated random
689 samples of radii based on the specified cell counts assuming a Gaussian distribution
690 with cell-type specific baseline mean and standard deviation: microglia = $2.0 \pm 0.5 \mu\text{m}$;

691 astrocytes and oligodendrocytes = $5.5 \pm 1.5 \mu\text{m}$; neurons = $8.0 \pm 2.0 \mu\text{m}$ for neurons
692 and $9.0 \pm 0.5 \mu\text{m}$ for endothelial. The resulting radii were concatenated to form a
693 comprehensive distribution and the MR apparent soma radius R_{soma} estimated as
694 $\left(\frac{R^5}{R^3}\right)^{1/2}$ as per Olesen et al. (2022).
695

696 **5. Data Availability**

697

698 Original datasets are accessible through the original publications, including the MICRA
699 (Koller et al., 2021) neuroimaging repeatability dataset (osf.io/z3mkn/), PsychENCODE
700 (<http://resource.psychencode.org/>) and BrainCloud
701 (https://www.ncbi.nlm.nih.gov/projects/gap/cgi-bin/study.cgi?study_id=phs000417.v2.p1).
702 Developmental MRI data are not available due to privacy concerns, however derived
703 data supporting the findings of the imaging analyses are available from the
704 corresponding author upon reasonable request.
705
706

707 **6. Code Availability**

708

709 Code for gene expression analysis will be made available at
710 github.com/garedaba/puberty-genes. TractSeg is available at [github.com/MIC-](https://github.com/MIC-DKFZ/TractSeg)
711 [DKFZ/TractSeg](https://github.com/MIC-DKFZ/TractSeg). MRtrix is available at www.mrtrix.org.
712

713 **7. Acknowledgements**

714

715 The authors would like to thank the families that participated in this study for their
716 generous contributions. We would also like to thank Umesh Rudrapatna and John
717 Evans for their assistance with acquisition protocols and Greg Parker and Simona
718 Schiavi for assistance with MRI processing. Figure 1 was created with
719 BioRender.com with elements from Macrovector via freepik.
720

721 The imaging data were acquired at the UK National Facility for In Vivo MR Imaging
722 of Human Tissue Microstructure funded by the EPSRC (grant EP/M029778/1), and
723 The Wolfson Foundation. SG and JYMY are supported by the Royal Children's
724 Hospital Foundation (RCHF 2022-1402). GB is supported by a National Health and
725 Medical Research Council Investigator Grant (1194497). EPR is supported by NICHD
726 at NIH (F32HD103313). CMWT is supported by a Veni grant (17331) from the
727 Dutch Research Council (NWO) and the Wellcome Trust (215944/Z/19/Z). MP is
728 supported by a UKRI Future Leaders Fellowship MR/T020296/2. DKJ is supported by

729 a Wellcome Trust Investigator Award (096646/Z/11/Z) and a Wellcome Trust Strategic
730 Award (104943/Z/14/Z).

731

732 **8. Author contributions**

733

734 SG, GB, MP and DKJ conceptualized the problem. SG, ER and IW acquired the
735 developmental MRI data. SG, MC and MP analyzed the MRI data. SG, GB and
736 MC performed statistical analyses. DKJ supervised and raised funding for this
737 project. SG wrote the original draft of the manuscript. All authors reviewed and
738 edited the manuscript.

739

740 **9. Competing interests**

741

742 The authors declare no competing interests.

743

744 **10. References**

745

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